



EVROPSKÁ UNIE
Evropské strukturální a investiční fondy
Operační program Výzkum, vývoj a vzdělávání

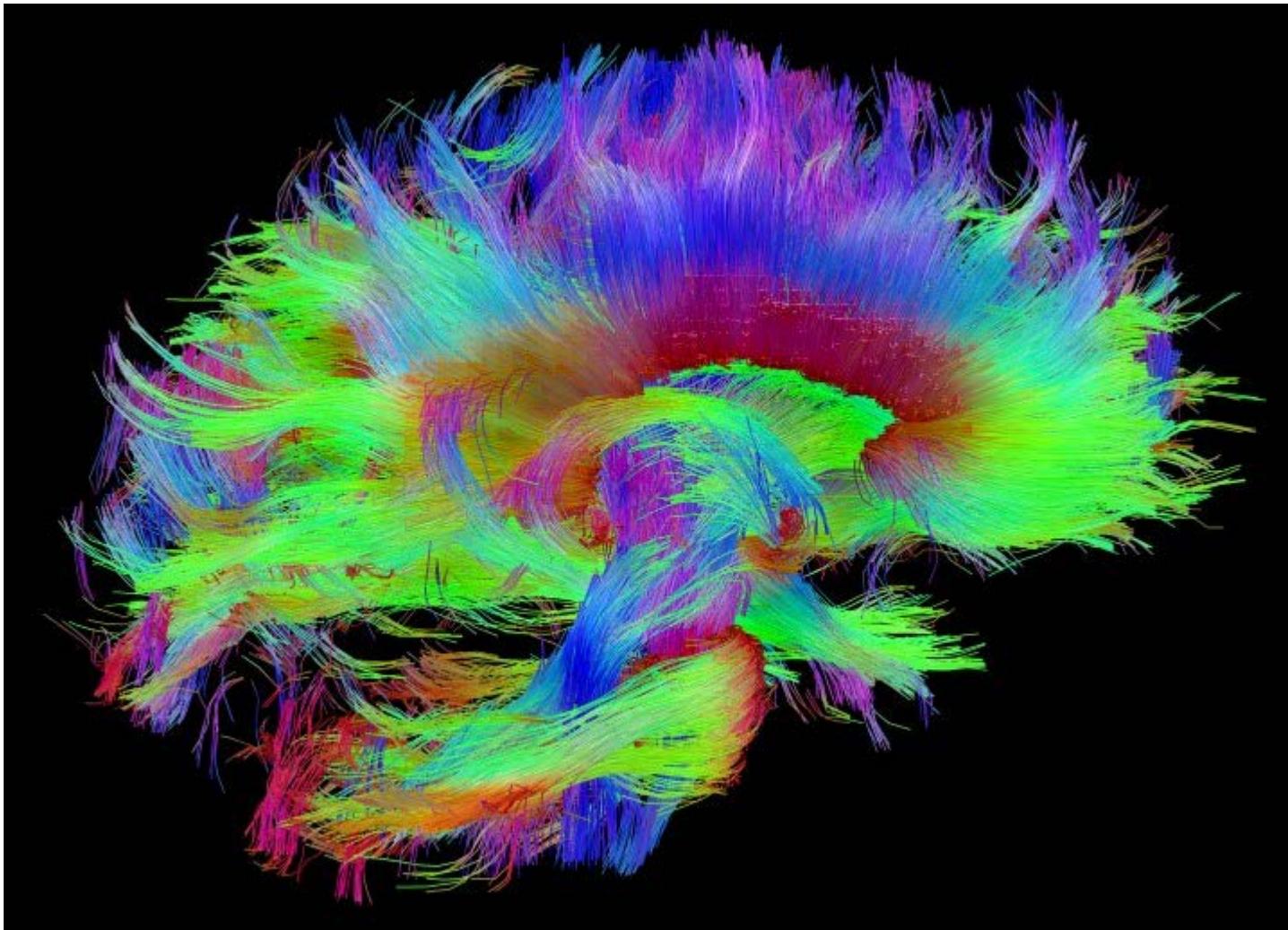


(Jaderná) Magnetická Rezonance

Diffusion Tensor Imaging - DTI

Zdroj: <https://predmety.fbmi.cvut.cz/cs/doktorske-bme>

Human Connectome Project



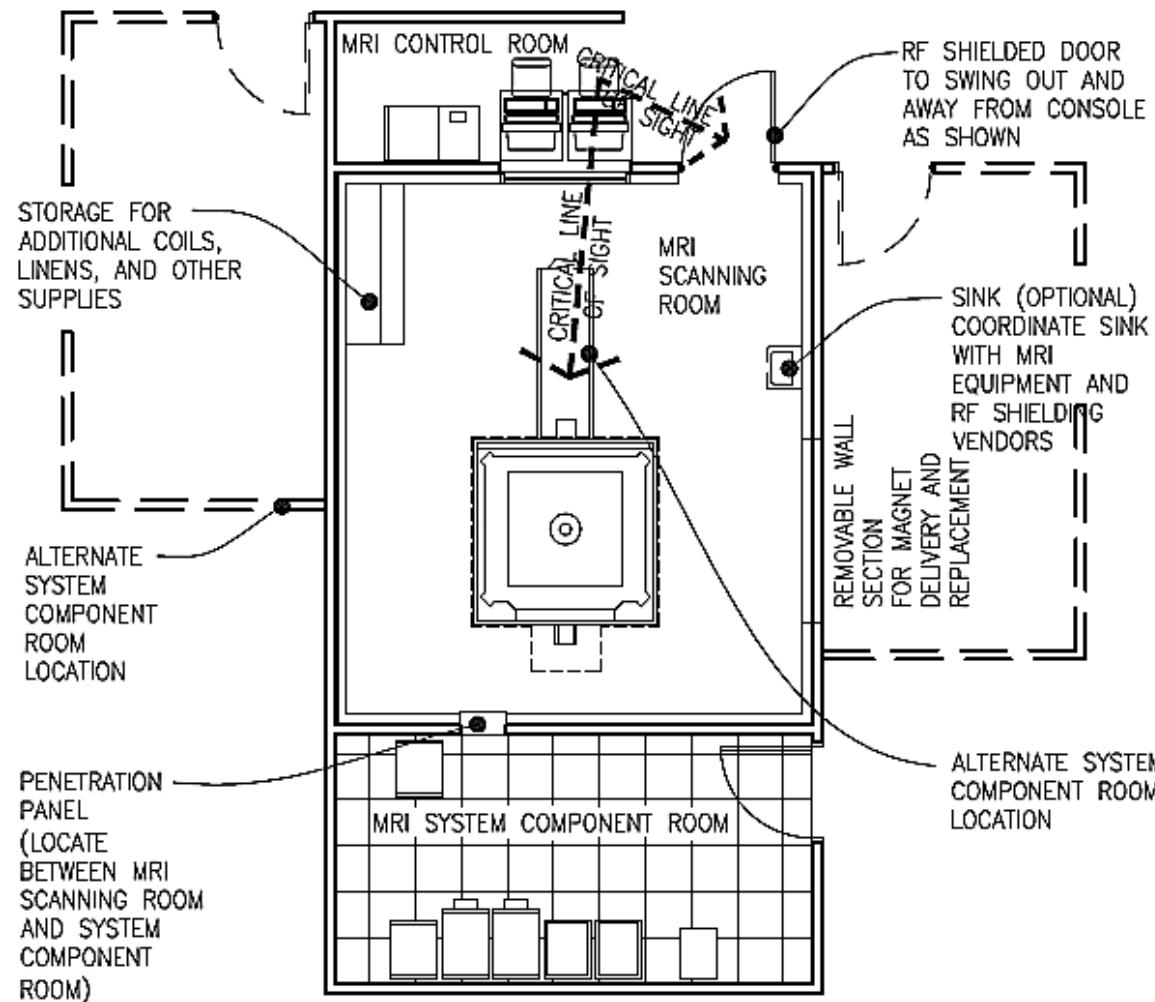
MRI přístroj – 7 T



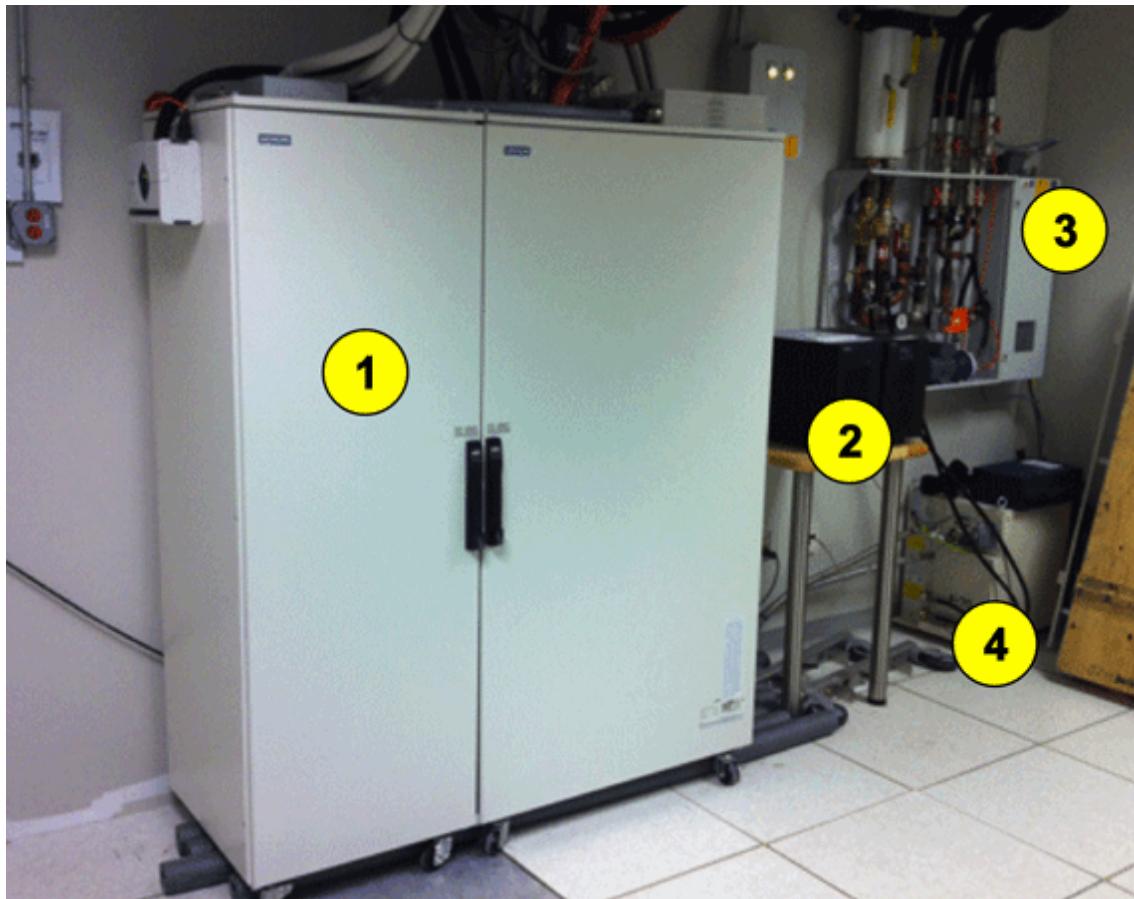
System weight (in operation)

<25 tons

MRI přístroj – instalace



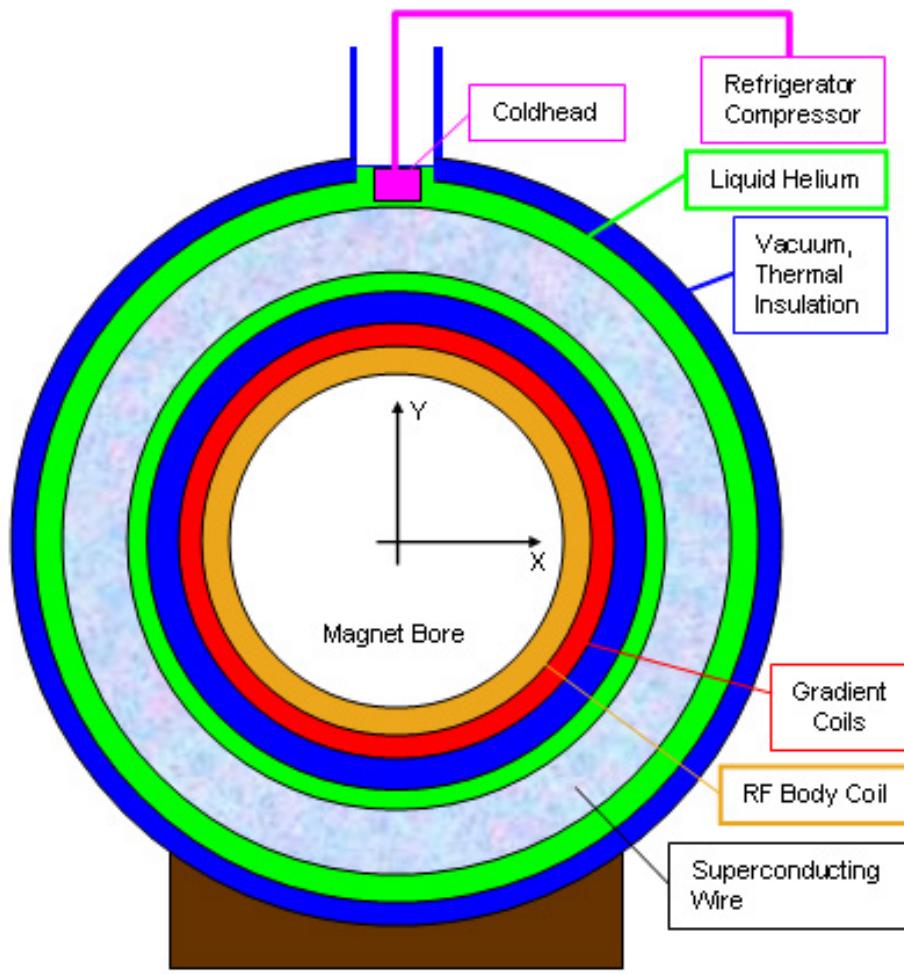
MRI přístroj – instalace



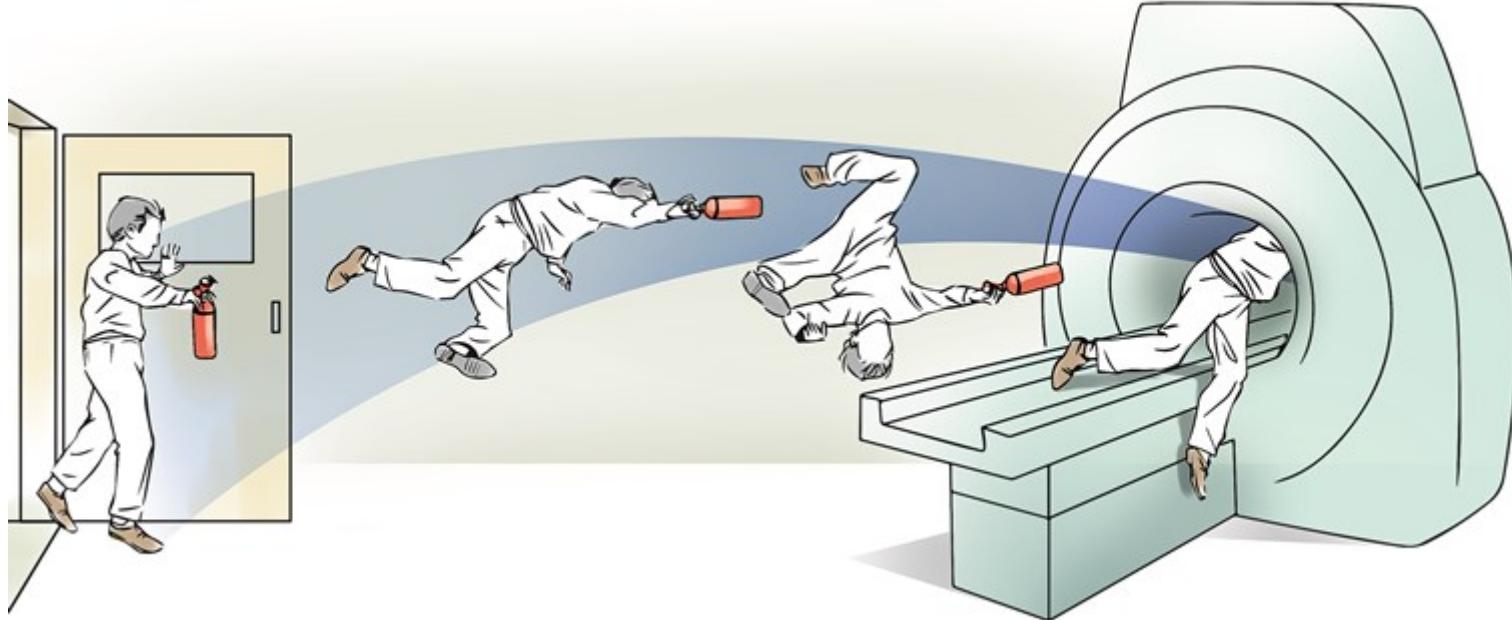
Cca 80 kVA (MRI)
v.
20 kVA (RD el. vyt.)

- 1) Gradient and radiofrequency cabinet; 2) universal power supply; 3) water pump/chiller; and 4) helium pump.

MRI přístroj - chlazení



MRI přístroj – kovové materiály

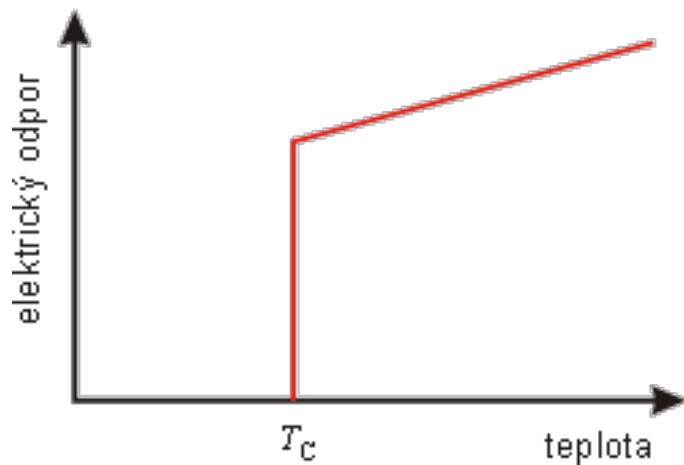


Červené tlačítko – Magnet quench: A quench refers to the sudden loss of superconductivity when its temperature is raised - <https://www.youtube.com/watch?v=9SOUJP5dFEg>

Základy fyziky

Základy fyziky – supravodivost

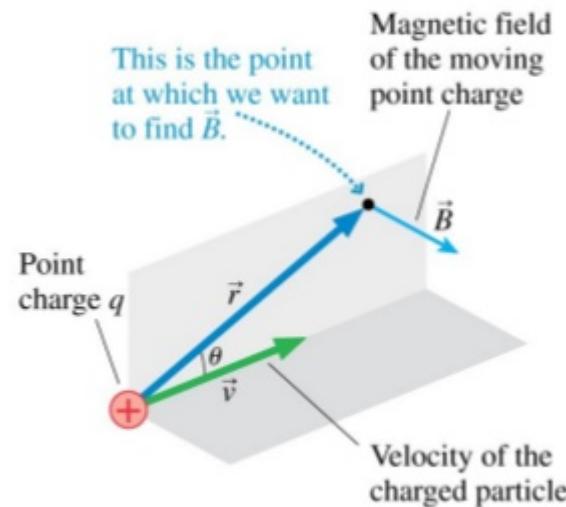
Supravodivost je jev kvantové mechaniky, při němž materiál ochlazený pod svou kritickou teplotu (T_C) vede elektrický proud bez odporu, takže se žádná energie neztrácí přeměnou na Jouleovo teplo.



Základy fyziky – Biot Savartův zákon

The source of the magnetic field: Moving charges

- The current in the wire consists of moving charges
- A moving charge alters the space to produce a magnetic field.
- A stationary charge will not produce a magnetic field

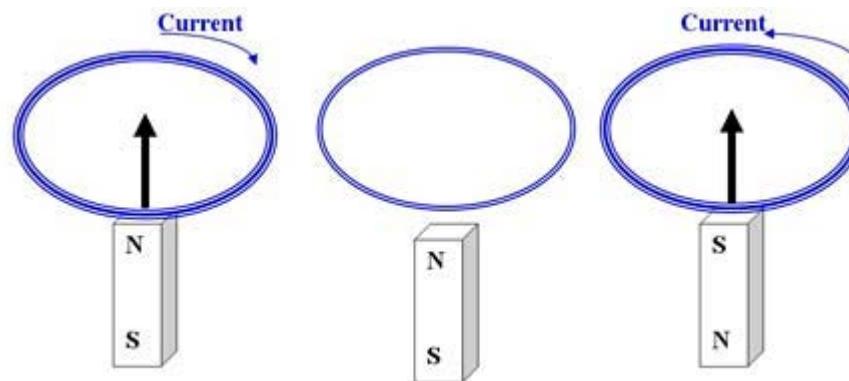


Ampérovo pravidlo pravé ruky

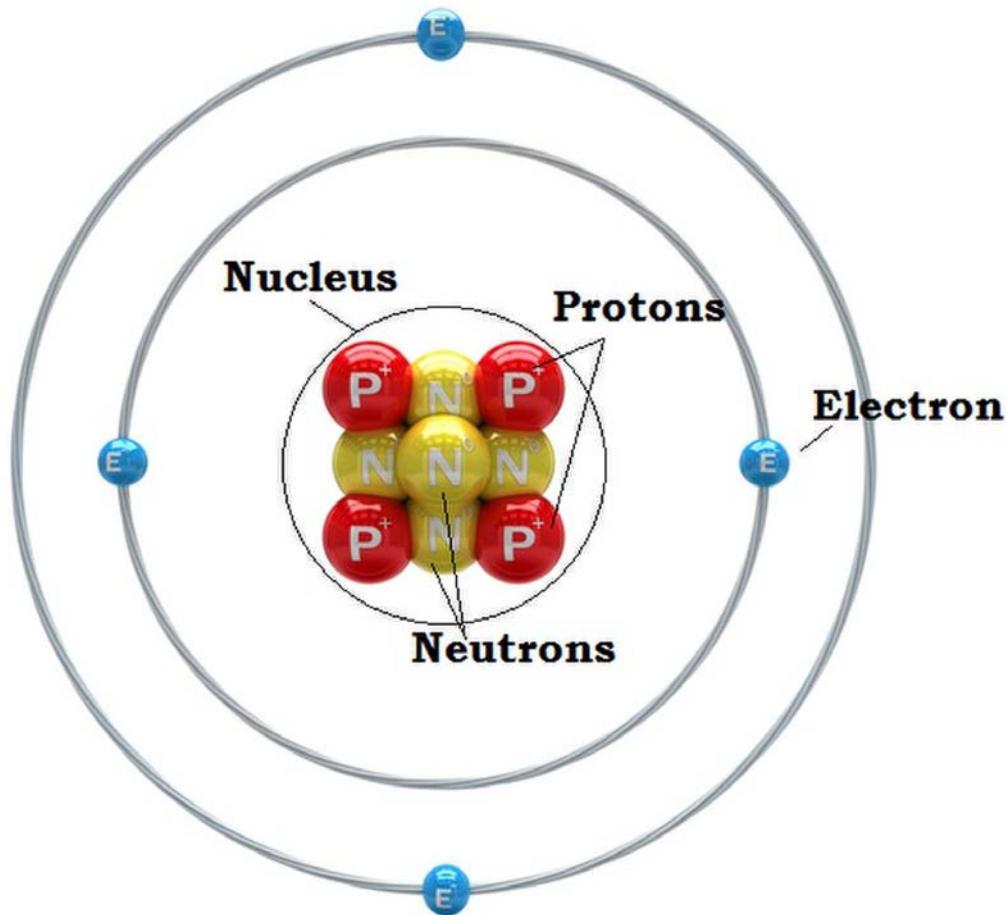
Základy fyziky – Faradayův zákon elektromagnetické indukce

Indukované elektromotorické napětí U_i je rovno záporně vzaté časové změně magnetického indukčního toku:

$$U_i = -\frac{\Delta \Phi}{\Delta t}$$



Základy fyziky – struktura atomu



Náboj:

$$1.6 \times 10^{-19} \text{ C}$$

$$-1.6 \times 10^{-19} \text{ C}$$

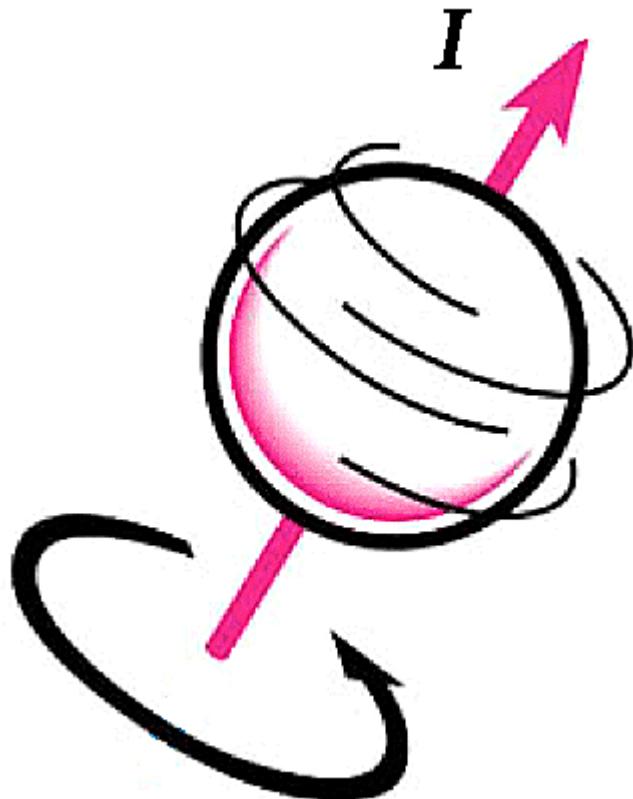
Hmotnost:

$$1.6749 \times 10^{-27} \text{ kg}$$

$$1.673 \times 10^{-27} \text{ kg}$$

$$9.109 \times 10^{-31} \text{ kg}$$

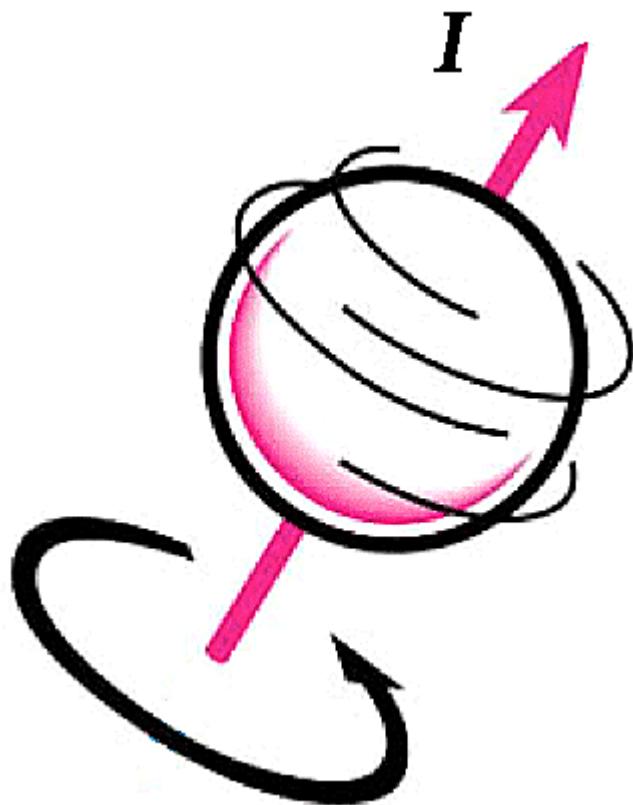
Fyzika částic - spin



Atomic and subatomic particles posses a corresponding property known as ***spin*** or ***spin angular momentum***. Protons, neutrons, whole nuclei, and electrons all possess *spin* and are often represented as tiny spinning balls.

Princip magnetické rezonance

Fyzika částic - spin



- **Proton and neutron spins** are known as nuclear spins.
- An unpaired component has a spin of $\frac{1}{2}$ and two particles with opposite spin cancel one another.
- **In NMR it is the unpaired nuclear spins that produce a signal in a magnetic field.**

Common Nuclei with NMR properties

- Criteria:

Must have ODD number of protons or ODD number of neutrons.

Reason?

It is impossible to arrange these nuclei so that a zero net angular momentum is achieved. Thus, these nuclei will display a magnetic moment and angular momentum necessary for NMR.

Examples:

^1H , ^{13}C , ^{19}F , ^{23}N , and ^{31}P with gyromagnetic ratio of **42.58**, 10.71, 40.08, 11.27 and 17.25 **MHz/T**.

Atomy a výsledný spin

Number of protons	Number of neutrons	Spin quantum number	Examples
Even	Even	0	^{12}C , ^{16}O , ^{32}S
Odd	Even	1/2	^1H , ^{19}F , ^{31}P
"	"	3/2	^{11}B , ^{35}Cl , ^{79}Br
Even	Odd	1/2	^{13}C
"	"	3/2	^{127}I
"	"	5/2	^{17}O
Odd	Odd	1	^2H , ^{14}N

Hydrogen

- Human body is mainly composed of fat and water, which makes the human body composed of about 63% hydrogen.
- Why Are Protons Important to MRI?
 - positively charged
 - spin about a central axis
 - a moving (spinning) charge creates a magnetic field.
 - the straight arrow (vector) indicates the direction of the magnetic field.

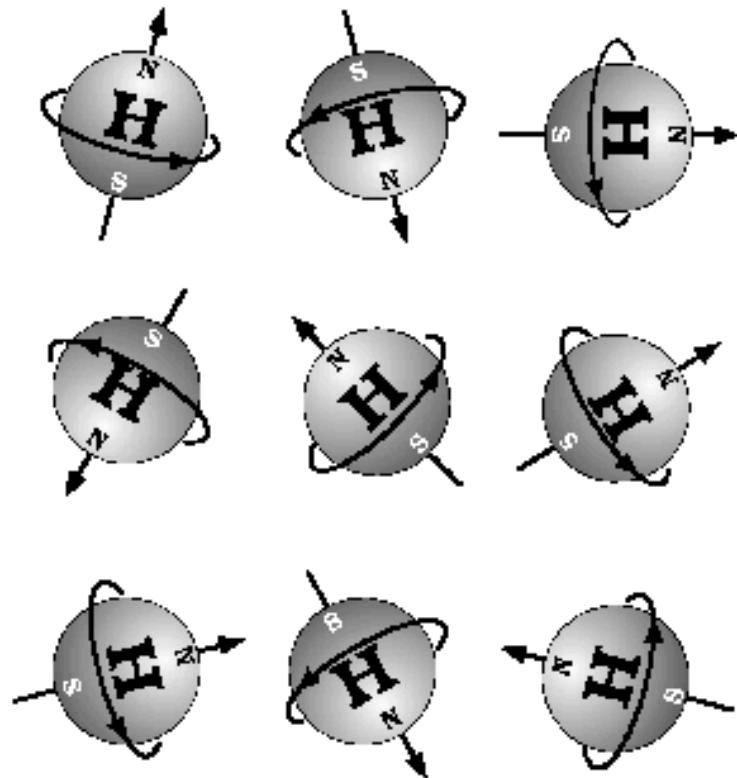


Example – 2 dcl water



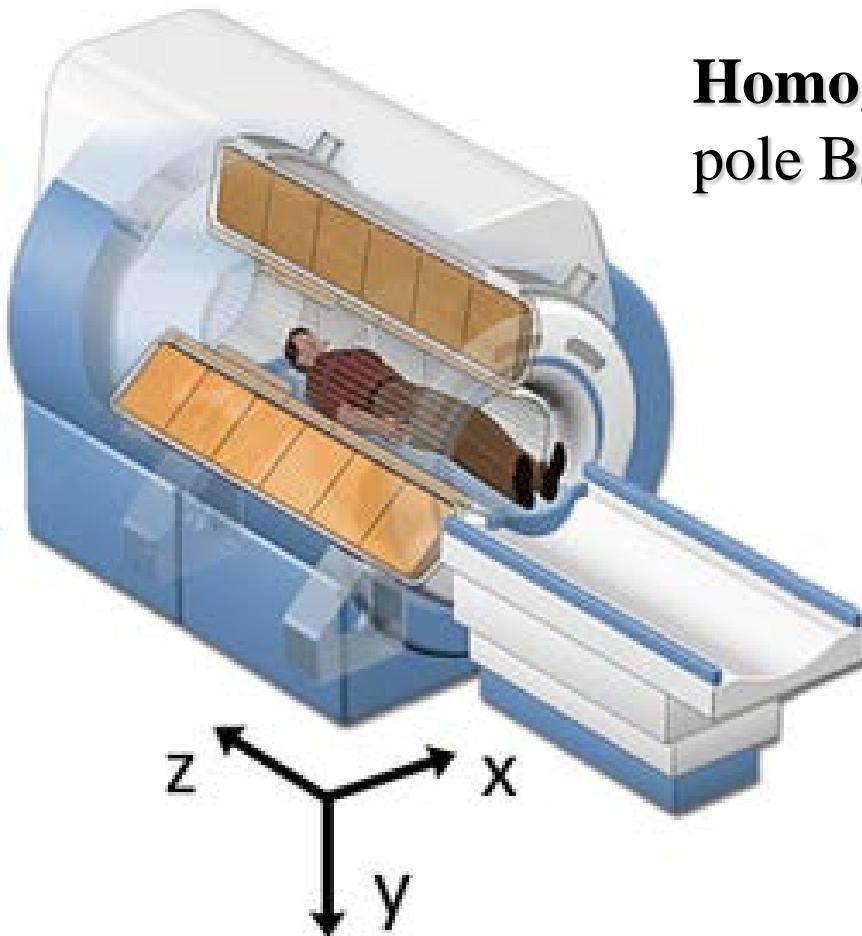
Protons of Hydrogen

*Spinning Protons Act
Like Little Magnets*



magnetické pole BO

MRI - coordinates

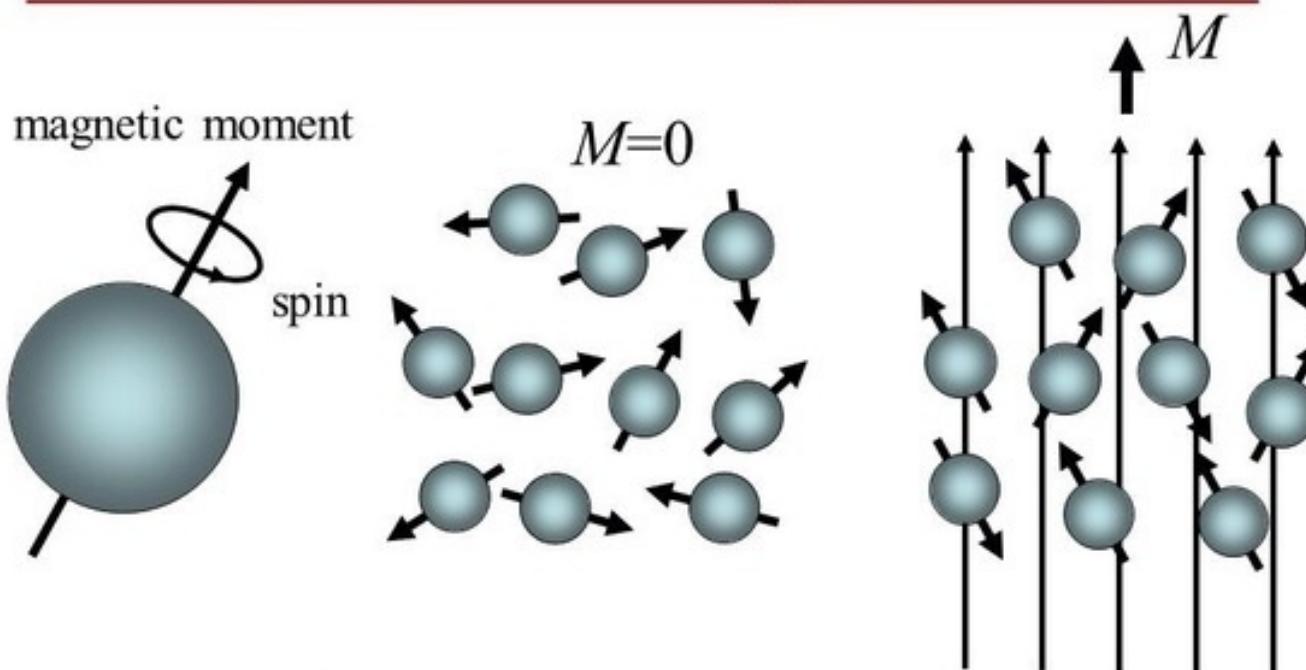


Homogenní magnetické pole B_0 ve směru osy z.

Homogenita mag. pole

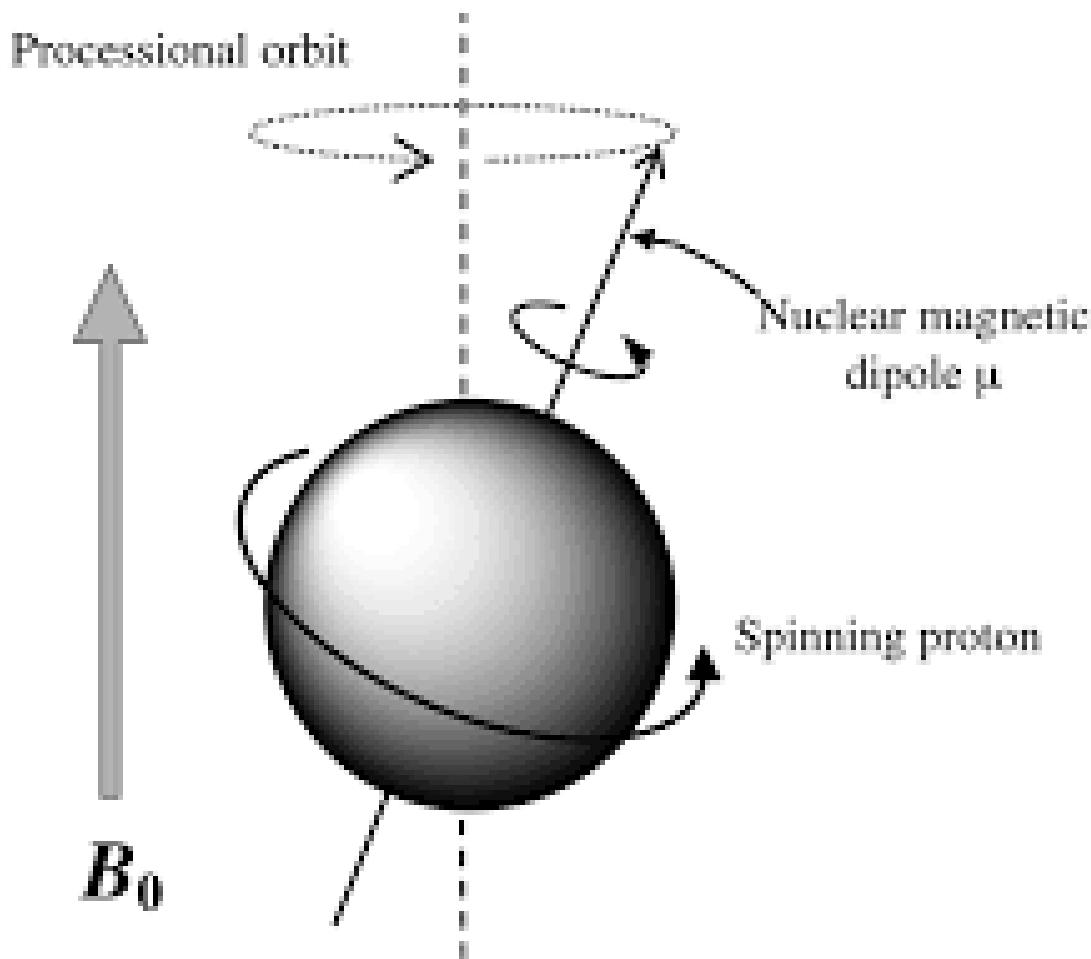
Protons of Hydrogen in B_0

Nuclear Spin



If a nucleus has an unpaired proton it will have spin and it will have a net **magnetic moment** or field

Precesní pohyb



Larmor Equation

- Frequency (rate) of precession is proportional to the strength of magnetic field

$$\omega = \gamma * B$$

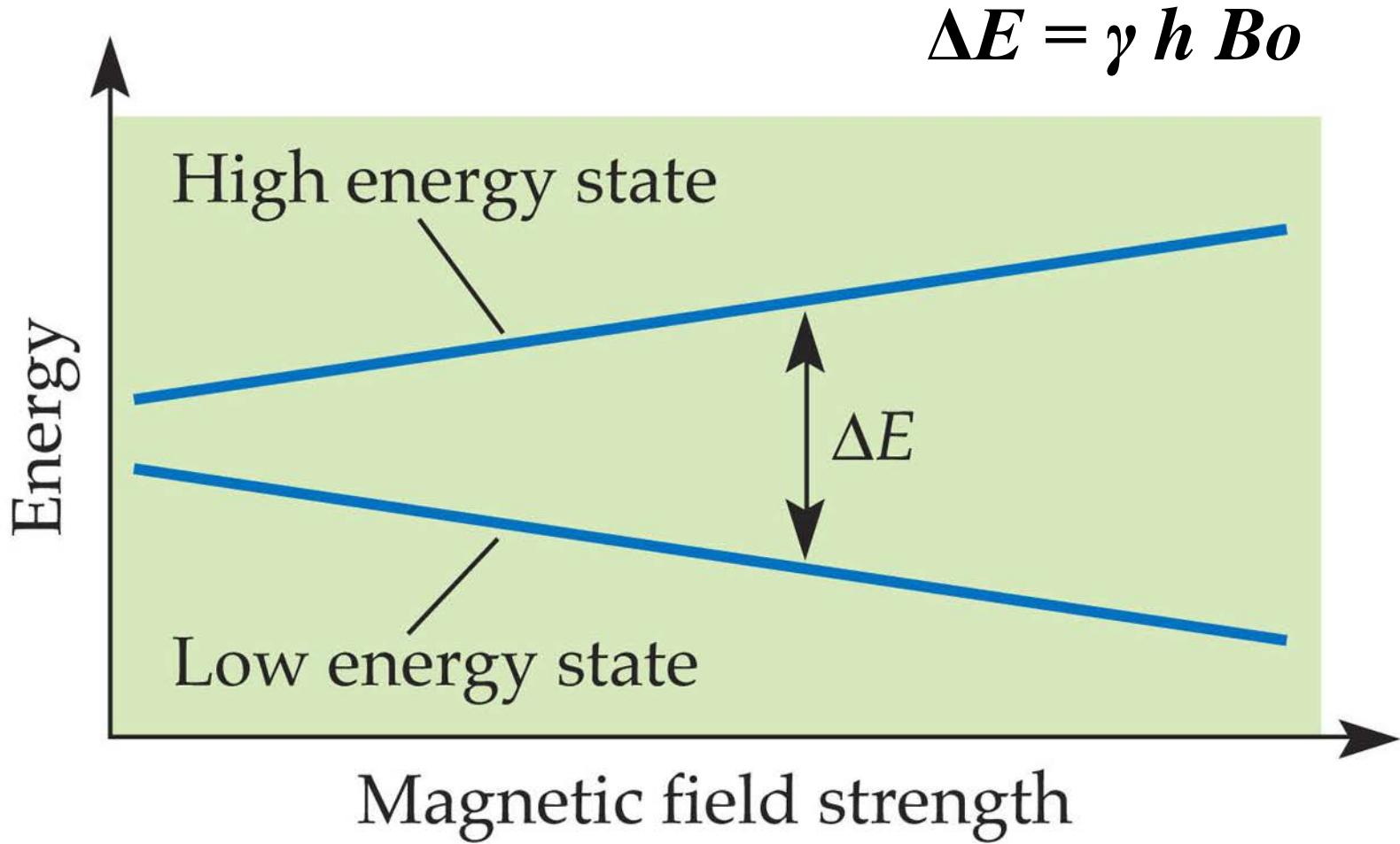
Larmor Frequency

$$\omega = \gamma * B$$

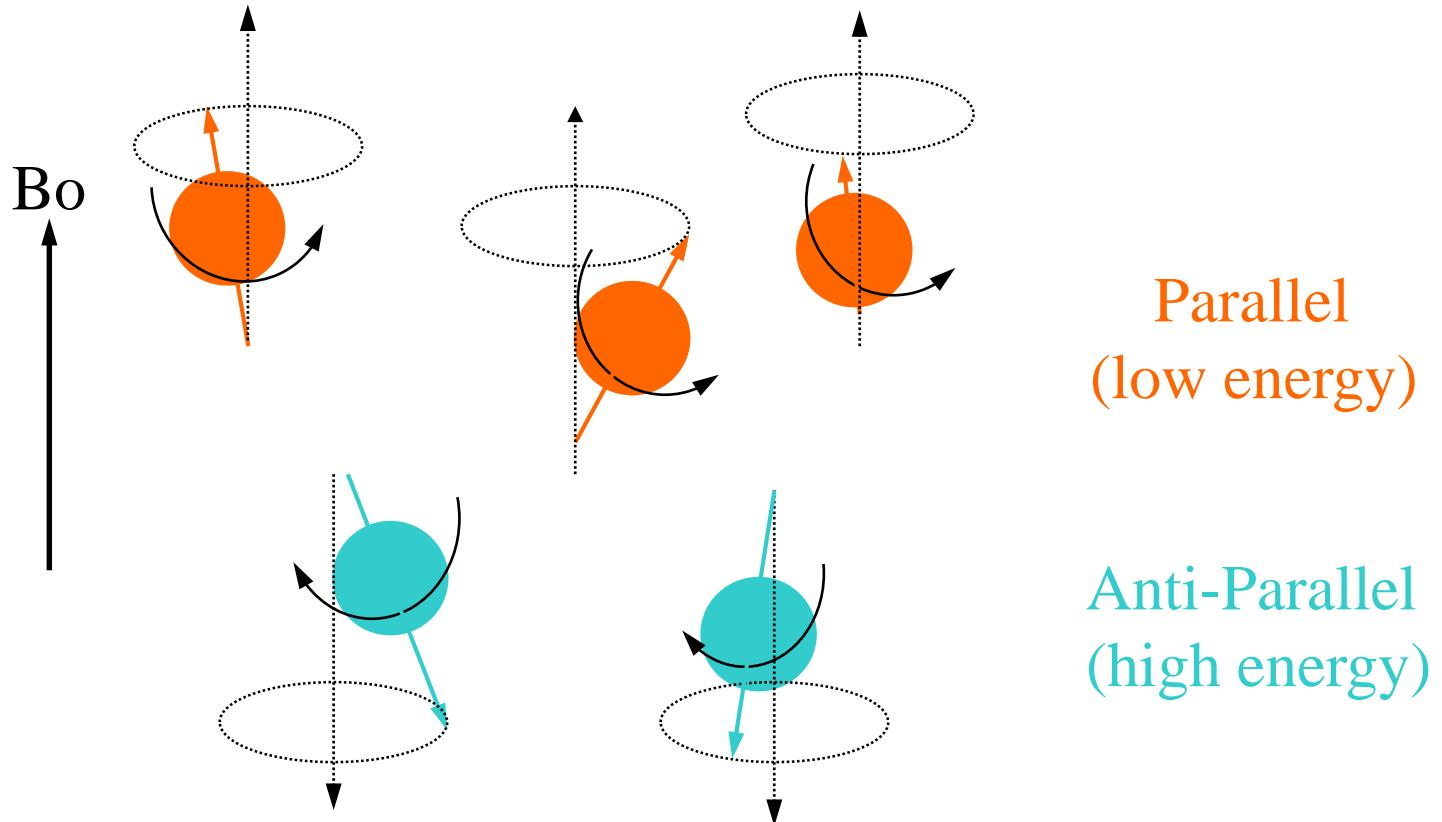
$$\omega = 63\text{MHz} \quad \text{If } B = 1.5\text{T}$$

$$\begin{aligned}\omega &= 2 * 63\text{MHz} \quad \text{If } B = 3.0\text{T} \\ &= 126\text{MHz}\end{aligned}$$

Zeeman Effect

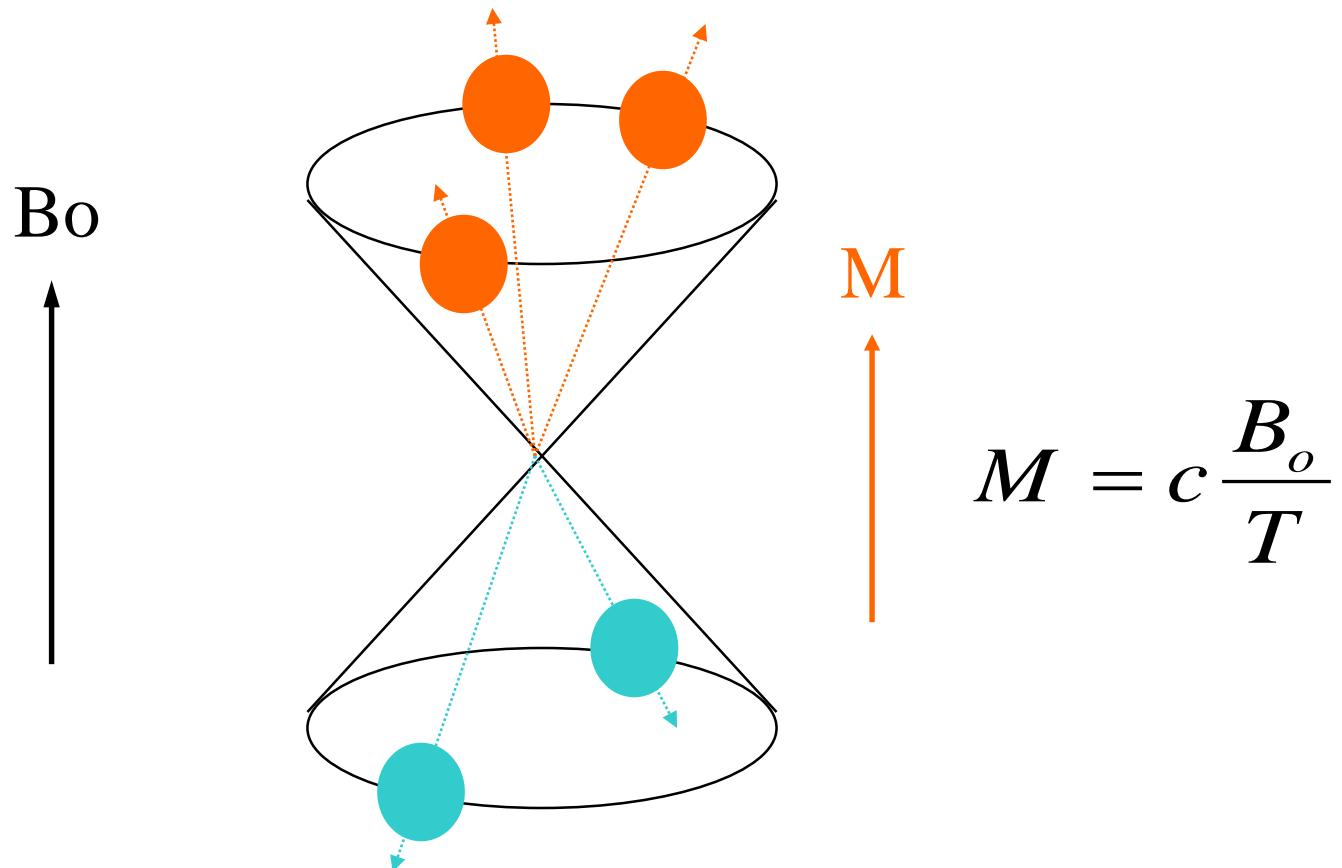


Protons in Magnetic Field B_0



Spinning protons in a magnetic field will assume two states.
If the temperature is 0° K , all spins will occupy the lower energy state.

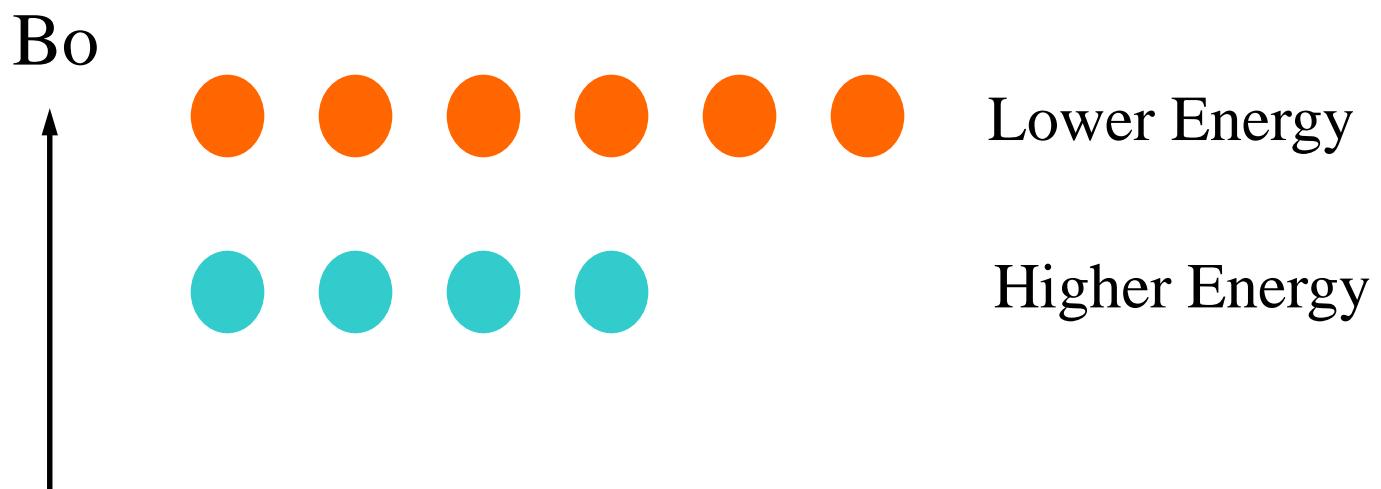
Net Magnetization



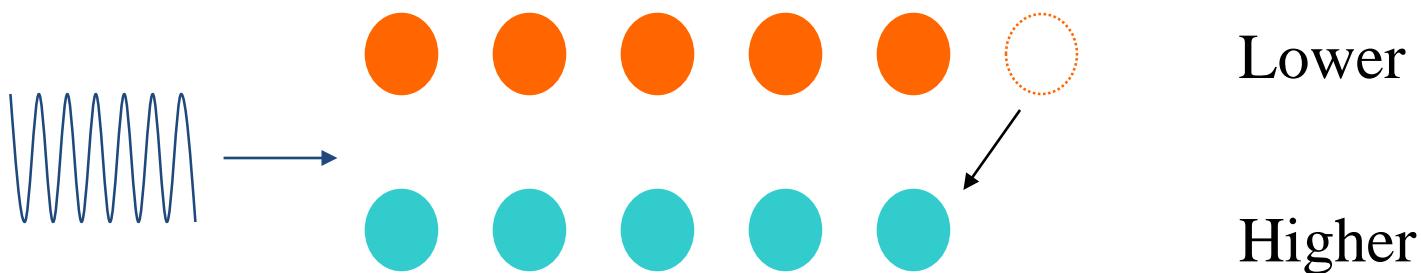
The Boltzmann equation describes the population ratio of the two energy states:

$$N^-/N^+ = e^{-\Delta E/kT}$$

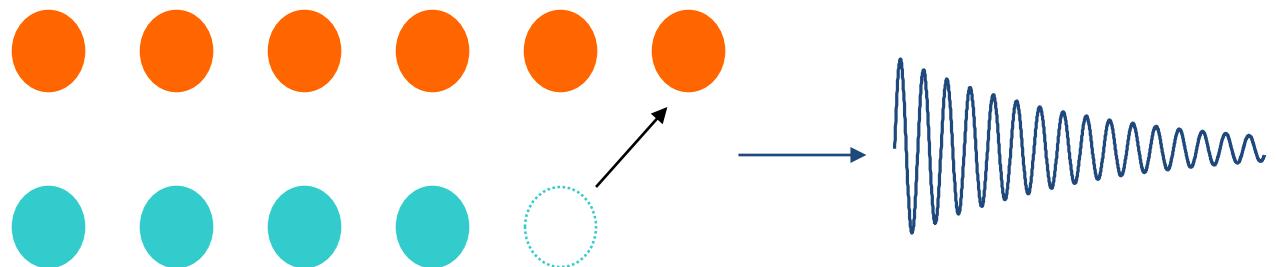
Spin System Before Irradiation



The Effect of Irradiation to the Spin System

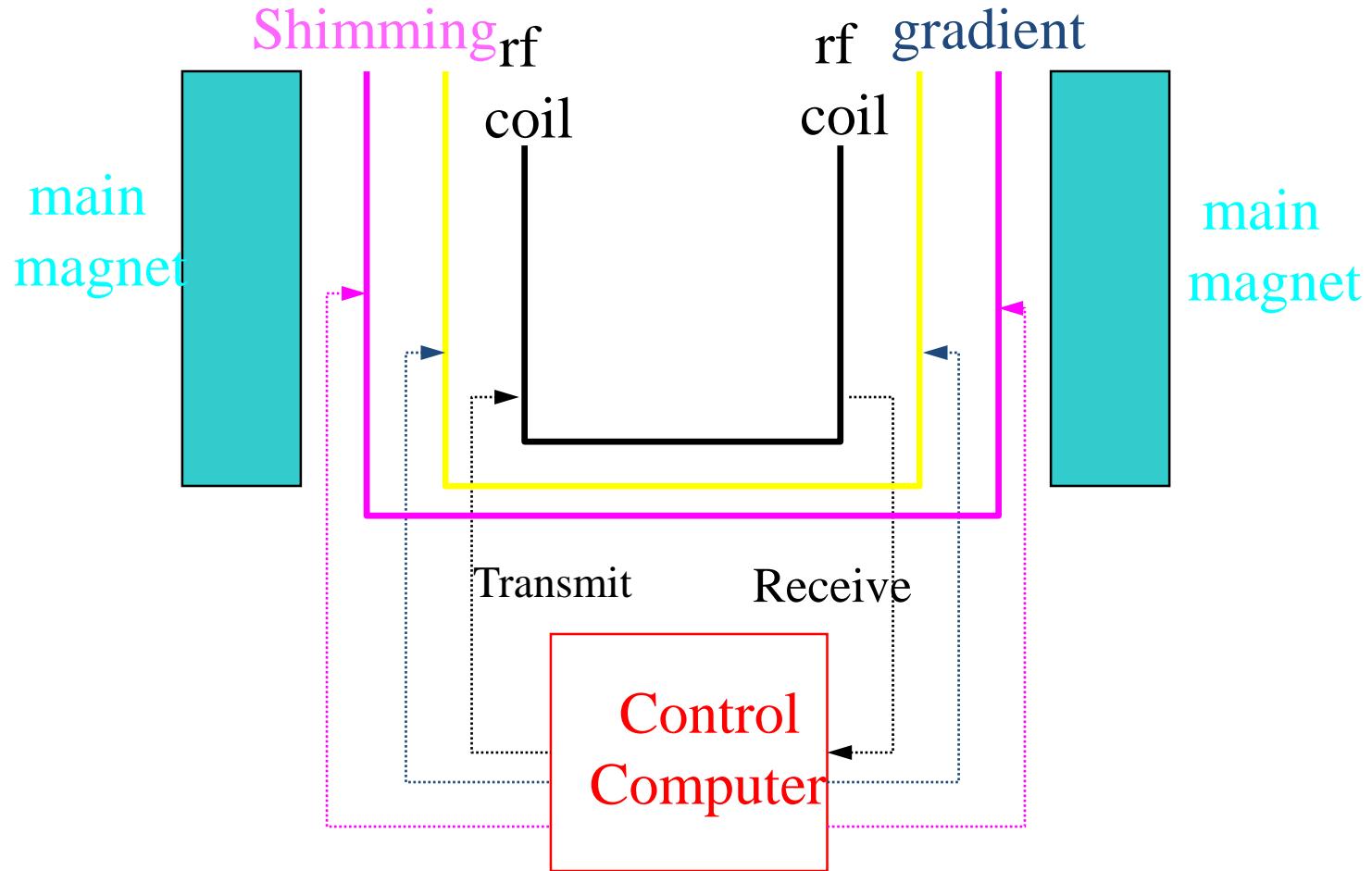


Spin System After Irradiation

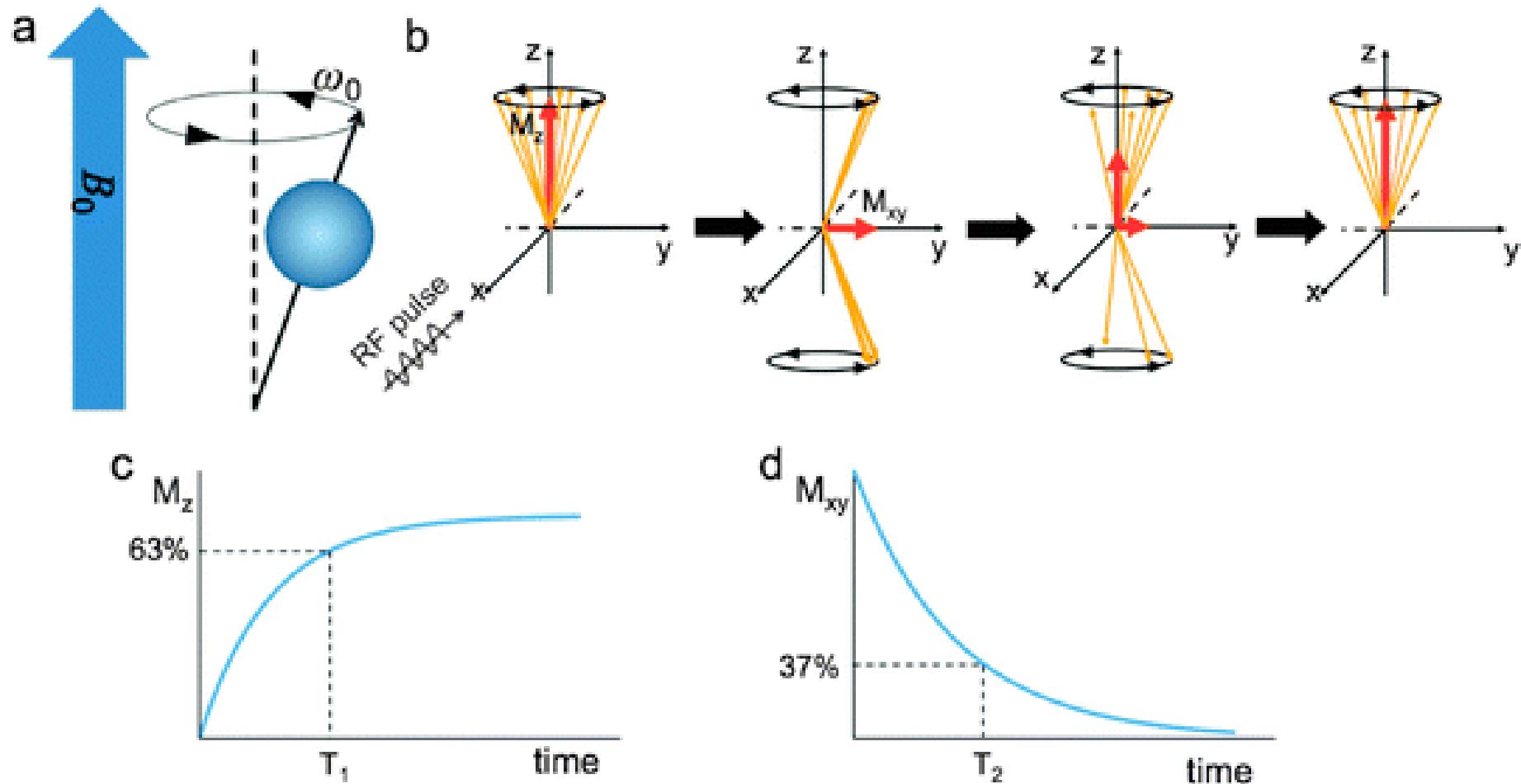


**RF a gradientní
cívky**

Components of MRI



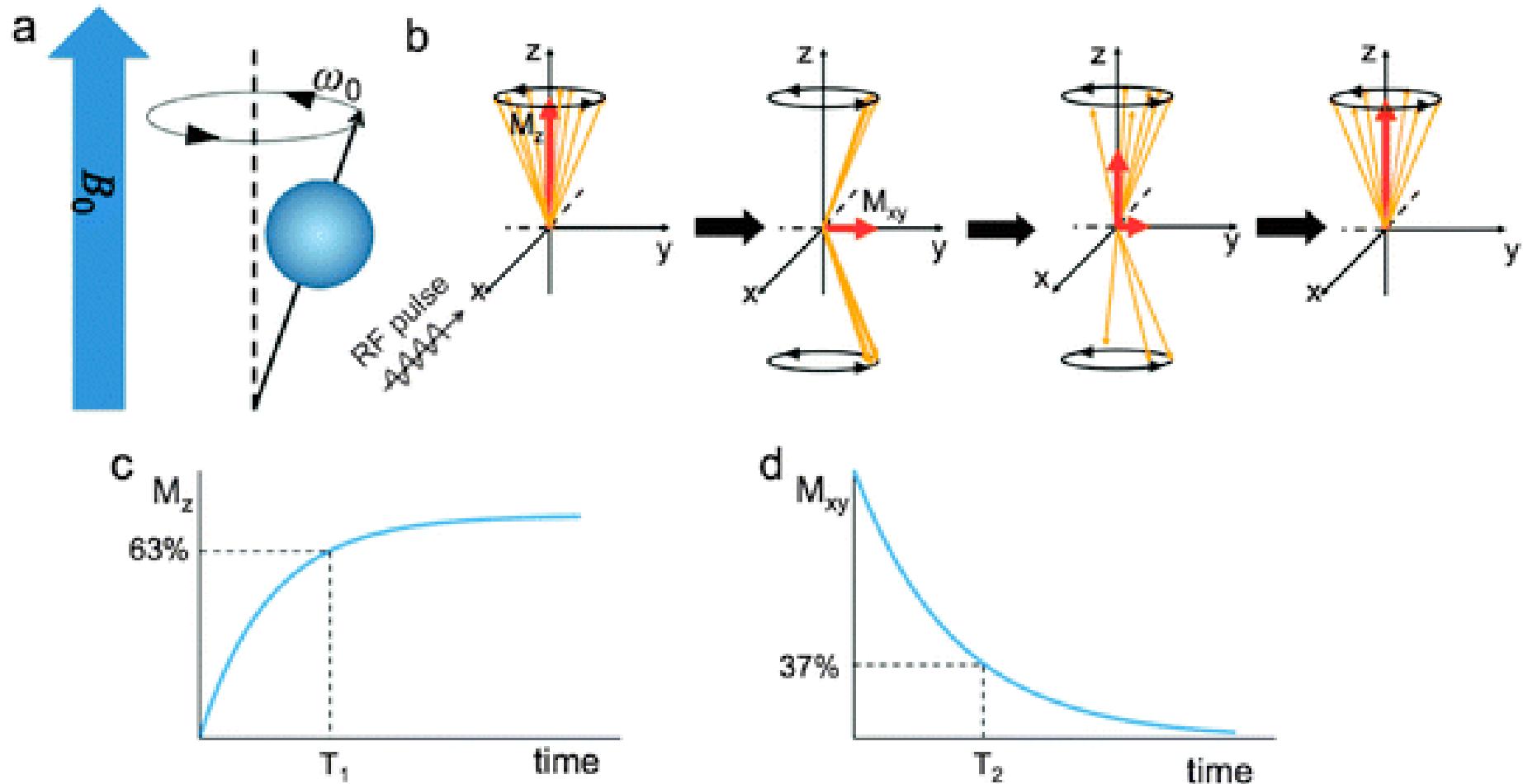
Radio-frequency pulse 90° – RF90



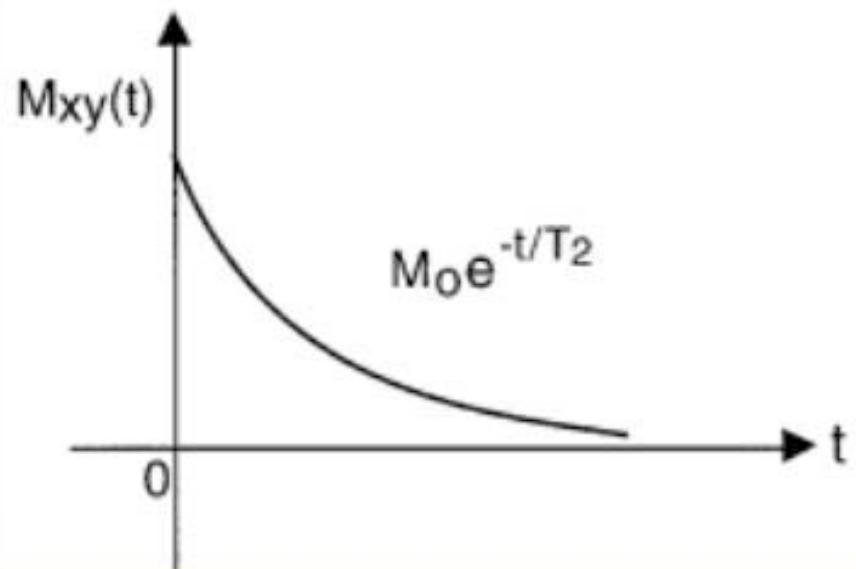
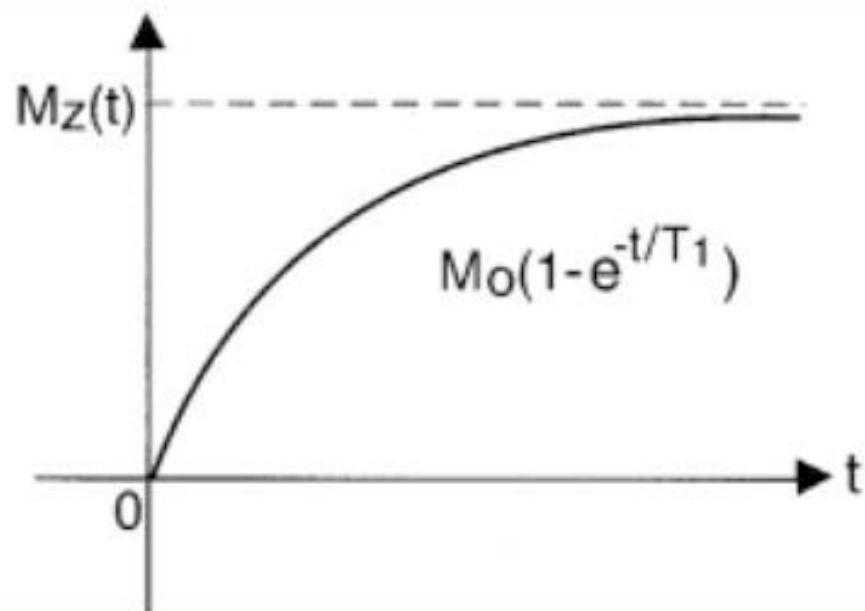
Types of Relaxation

- *Longitudinal* – precessing protons are pulled back into alignment with main magnetic field of the scanner (B_o) reducing size of the magnetic moment vector in the x-y plane
- *Transverse* – precessing protons become out of phase leading to a drop in the net magnetic moment vector (M_o)
- Transverse relaxation occurs much faster than Longitudinal relaxation
- *Tissue contrast is determined by differences in these two types of relaxation*

Relaxations



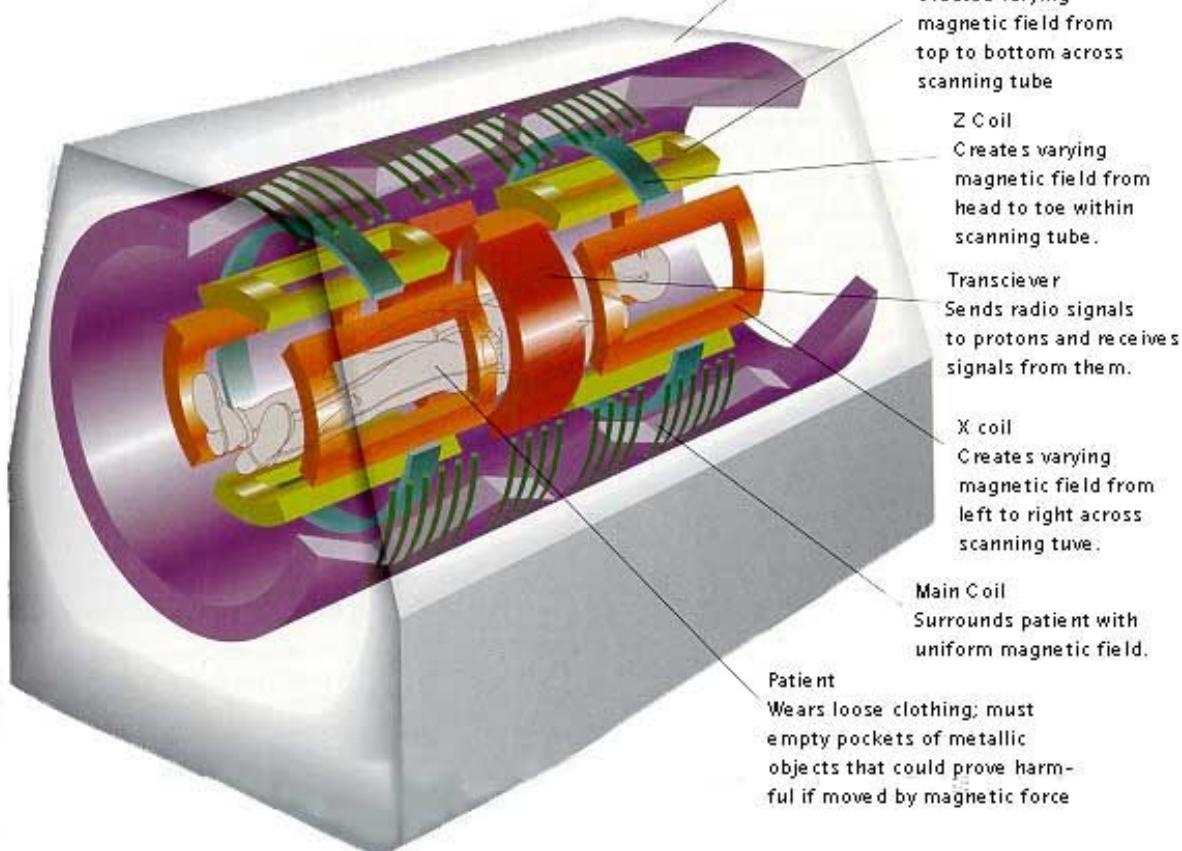
Magnetization – PD, T1, T2



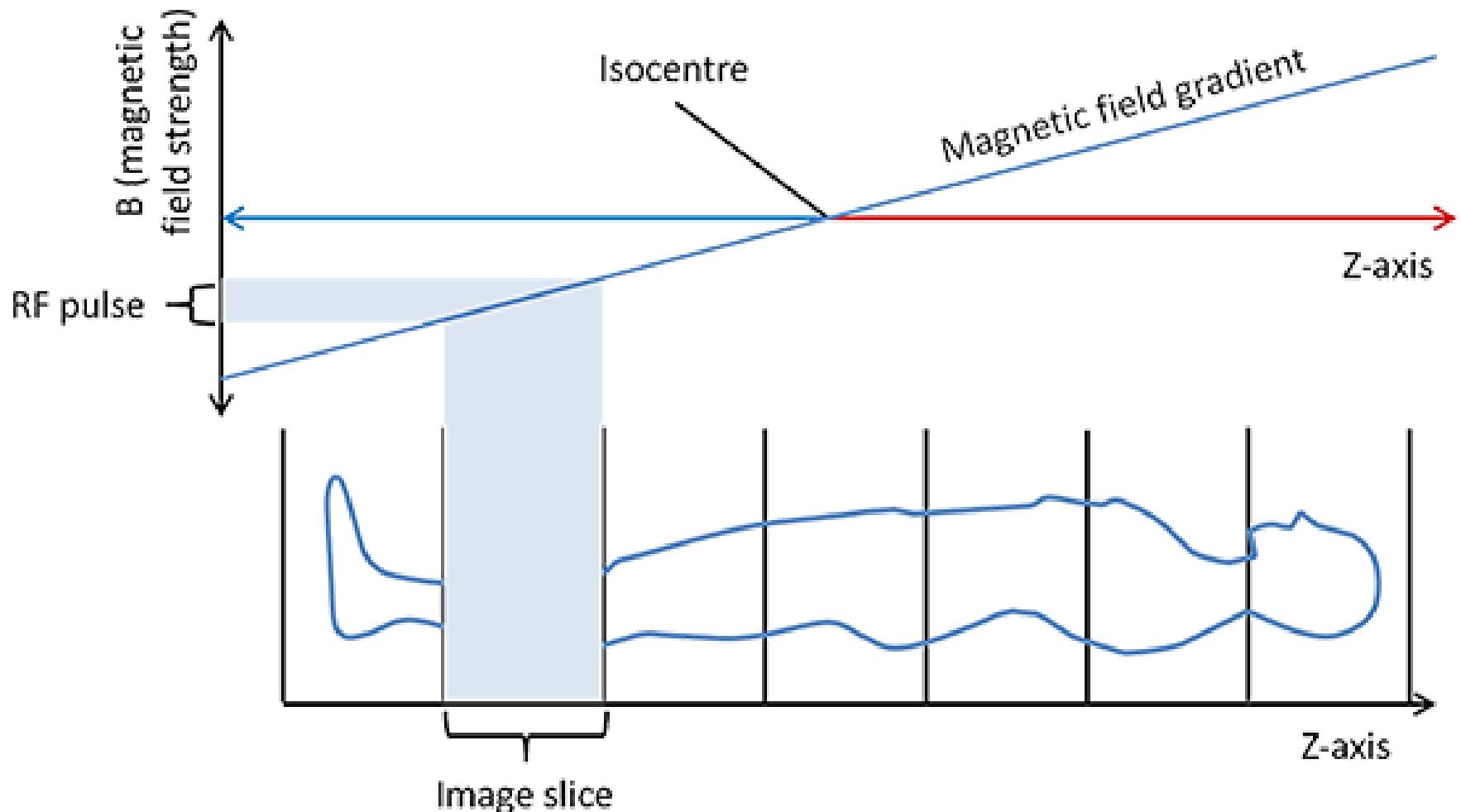
Gradient coils

CREATING Refined ANATOMICAL IMAGES

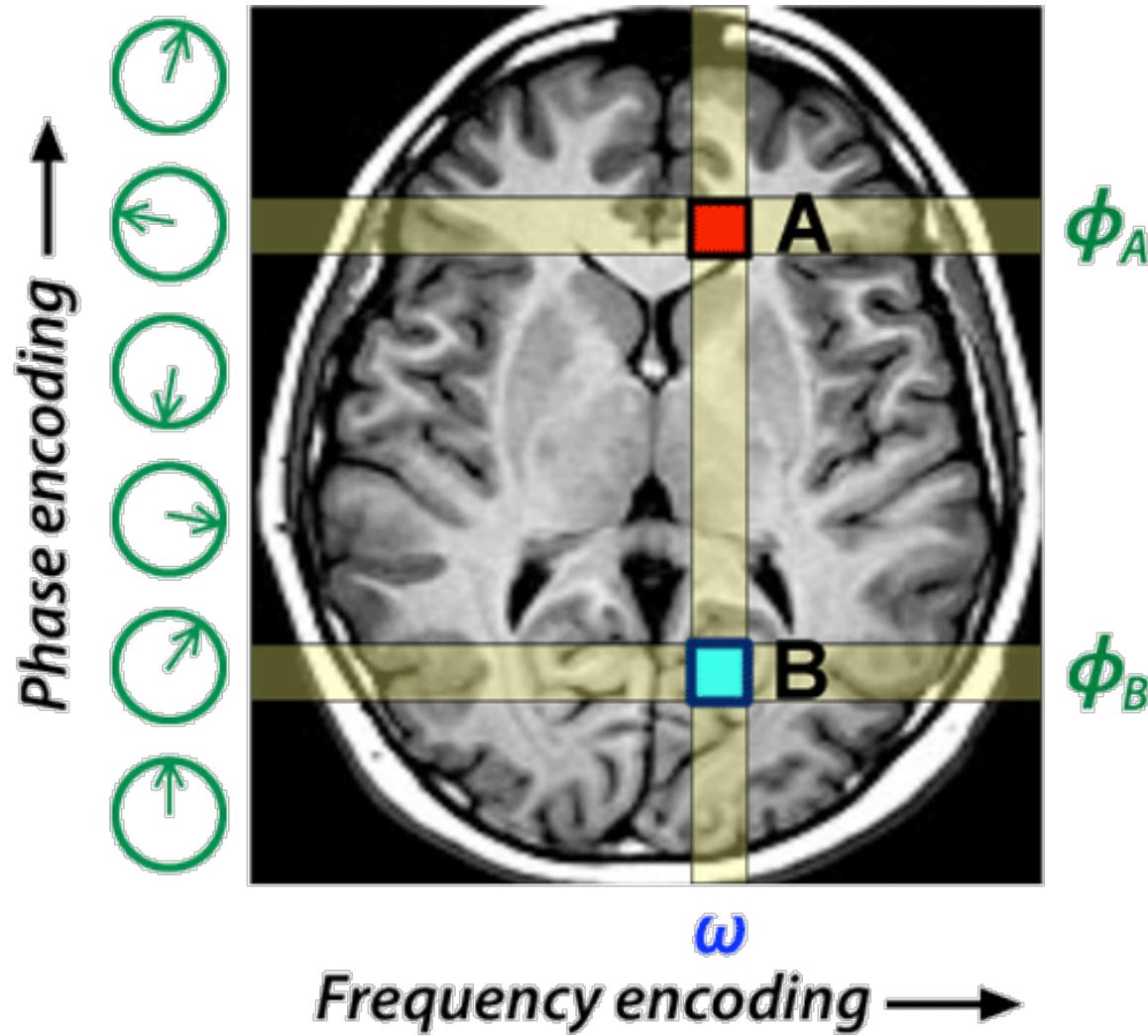
Within the metallic cocoon of an MRI scanner,
the patient is surrounded by four electromagnetic
coils and the components of a transciever



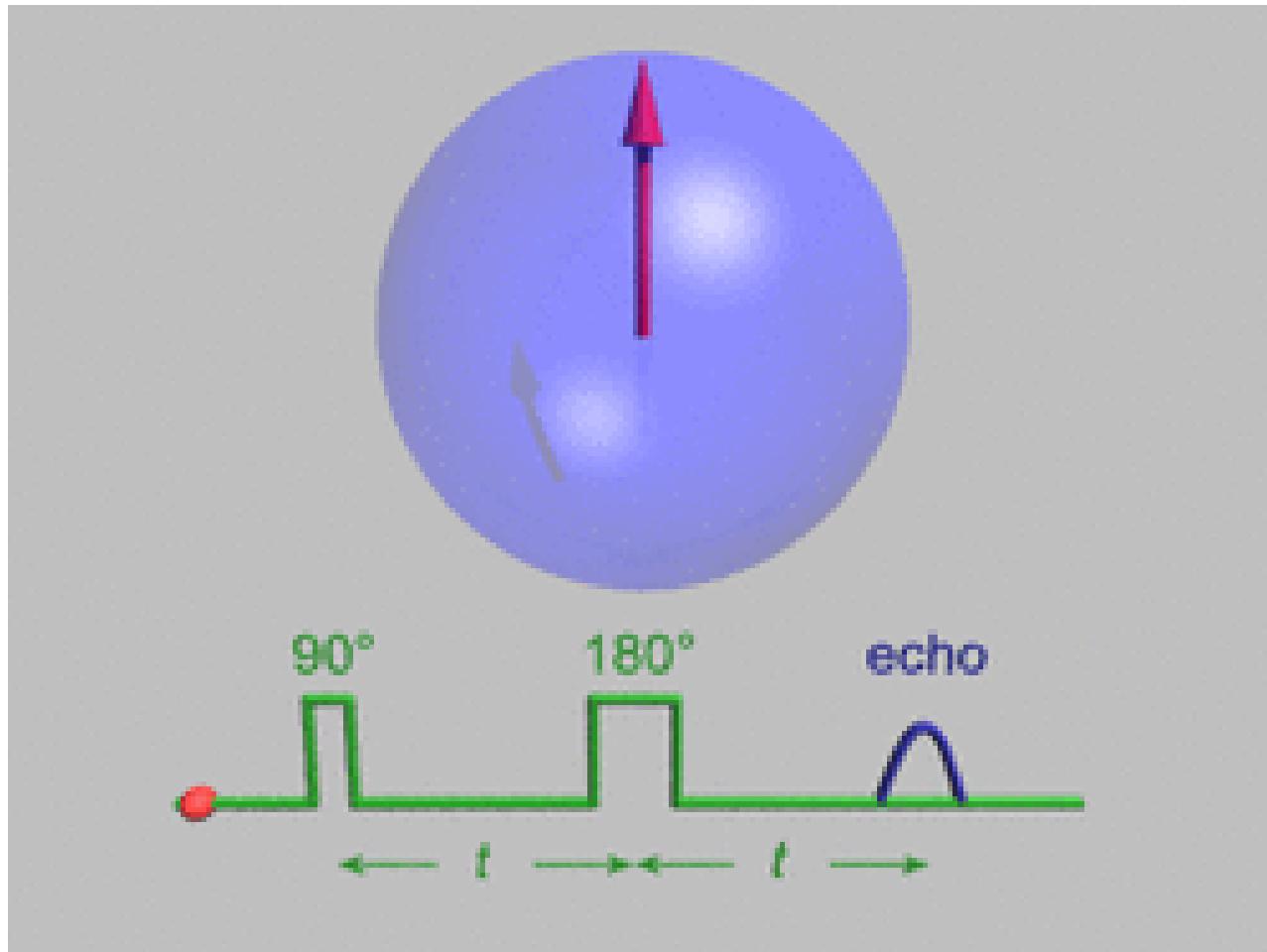
Výběr řezu



Prostorové kódování



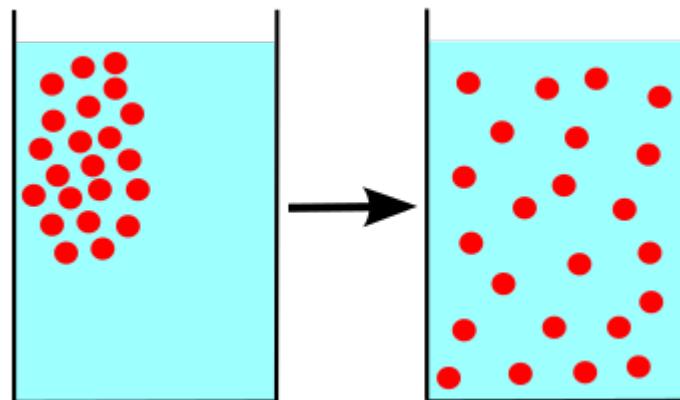
Spin echo sekvence



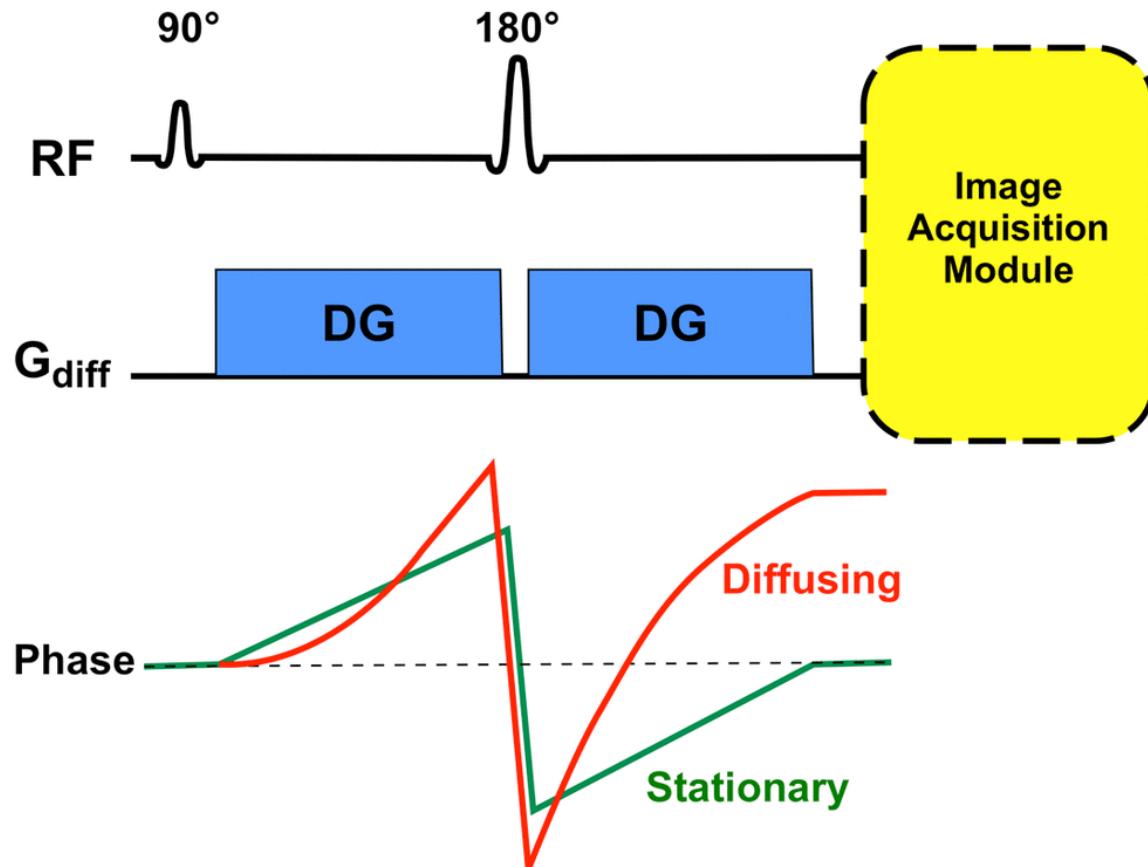
Fyzika pro DÚI

Difuze

Látky přecházejí samovolně (náhodným pohybem) z prostředí, kde je jejich koncentrace vyšší směrem tam, kde byla dosud jejich koncentrace nižší. Nedifunduje jen jedna látka do druhé. Proces je pro látku a rozpouštědlo vzájemný.



Diffusion Weight Imaging



Stationary spins are not affected by the paired gradients, but diffusing spins are dephased.

Fyzika pro DTI

Fyzika pro DTI

Izotropní prostředí

- kámen vložený do vody:
 - na vodní hladině vznikají kruhové vlny
 - kruhový tvar svědčí o stejné rychlosti vlnění ve všech směrech
 - prostředí má ve všech směrech stejně vlastnosti
 - izotropní prostředí**
 - za dobu t se vytvoří na vodní hladině kružnice o poloměru r
 - $r = v \cdot t$
 - všechny body na této kružnici mají stejnou fázi
 - podobně se šíří i mechanické vlnění včetně zvuku
- rychlosť světla nezávisí na směru šíření (sklo)

Fyzika pro DTI

Anizotropní prostředí

- opticky anizotropní prostředí - rychlosť svetla závisí na smere Šíření (krystal křemene)
- **Anizotropie** je vlastnosť, ktorou sa označuje závislosť určitej veličiny na volbe smere.
- Biological tissues are highly anisotropic, meaning that their diffusion rates are *not* the same in every direction.

Fyzika pro DTI

Skalár se skládá z čísla a fyzikální jednotky.

Mezi skaláry patří např. termodynamická teplota (100 K), délka (10 m), objem (2 m³), ale i hmotnost (3 kg) atd.

Vektory jsou fyzikální veličiny, které jsou kromě velikosti určeny také směrem.

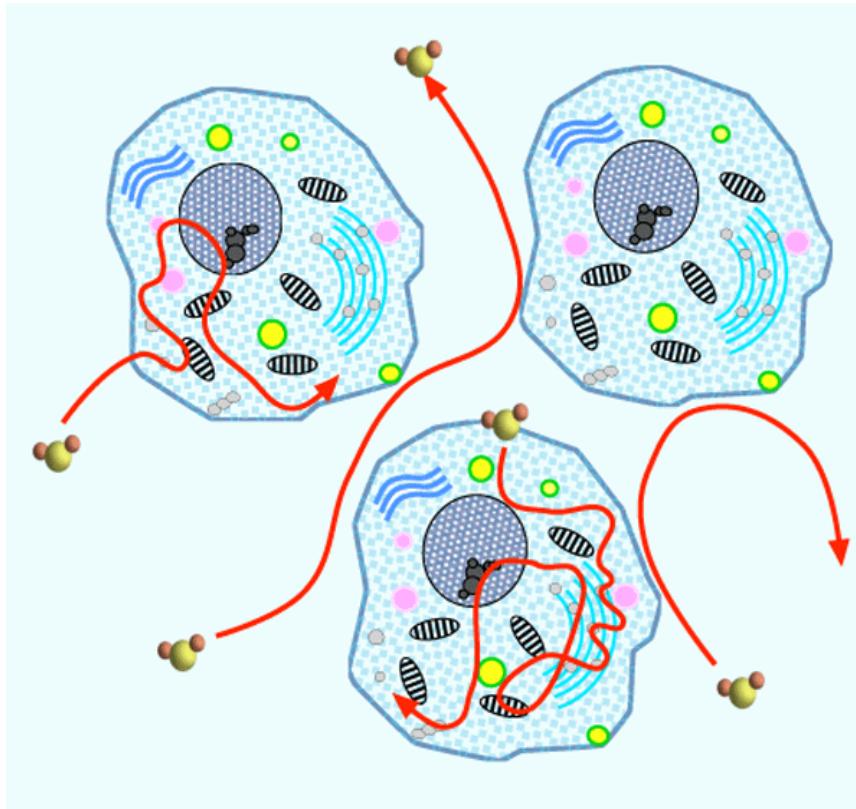
Většinou označujeme vektor šipkou nad příslušným písmenem. Mezi vektorové veličiny patří např. okamžitá rychlosť v , síla F atd.

Fyzika pro DTI

Tenzor

Patří mezi fyzikální veličiny, které mají složitější strukturu než vektory. **Obecně není názorná interpretace tenzoru možná**, ale je možné si ji u kázat alespoň na několika konkrétních příkladech. Mezi tenzorové veličiny patří např. tenzor napětí nebo tenzor deformace.

Difuze molekul vody



Diffusion of water molecules (red arrows) is hindered in the intracellular compartment due to the presence of macromolecules, increased viscosity, and multiple membranes. Only mild restriction of diffusion (due principally to tortuosity) occurs in the extracellular space.

Diffusion tensor

Biological tissues are highly anisotropic, meaning that their diffusion rates are *not* the same in every direction.

Diffusion Tensor

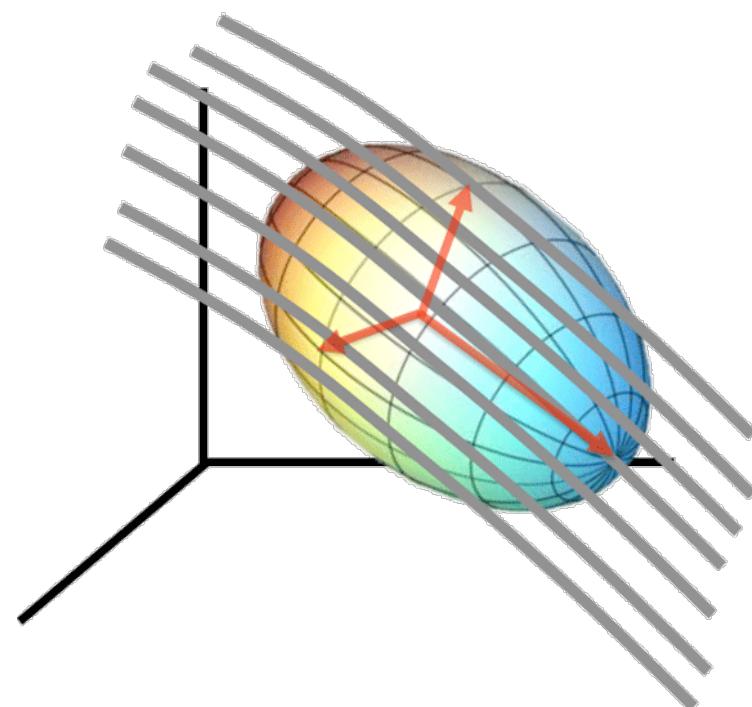
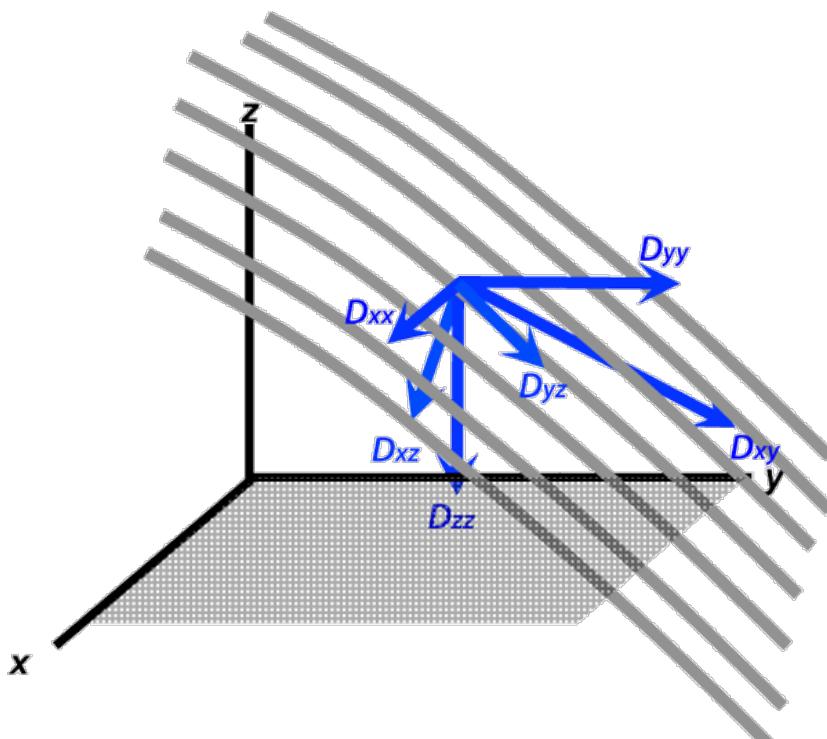
$$\mathcal{D} = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{yx} & D_{yy} & D_{yz} \\ D_{zx} & D_{zy} & D_{zz} \end{bmatrix}$$

$$\mathcal{D}_{isotropic} = \begin{bmatrix} D & 0 & 0 \\ 0 & D & 0 \\ 0 & 0 & D \end{bmatrix}$$

The values we calculate for each tensor component (such as D_{xx} or D_{xy}), however, are not unique, being dependent on the (x - y - z) frame of reference chosen for measurement. Had we selected a different coordinate system (x' - y' - z') not aligned with the patient but at some arbitrary angle, the calculated values ($D_{x'x'}$ or $D_{x'y'}$) would have been completely different.

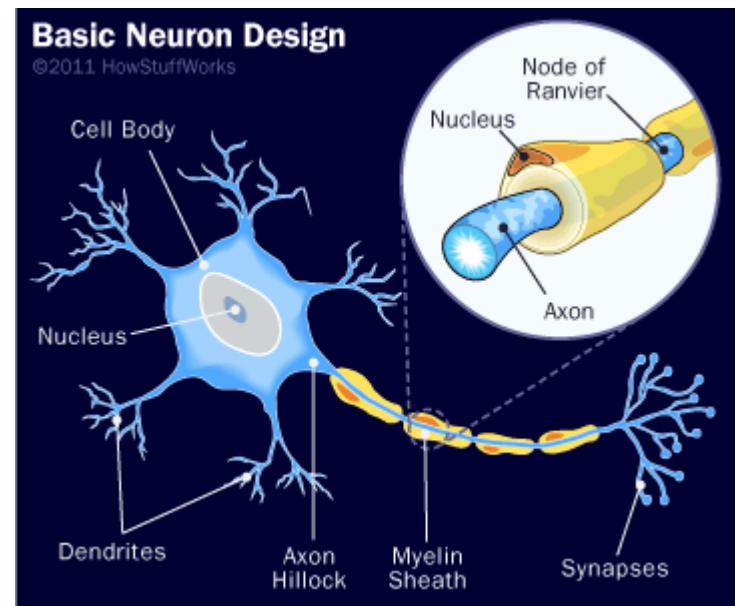
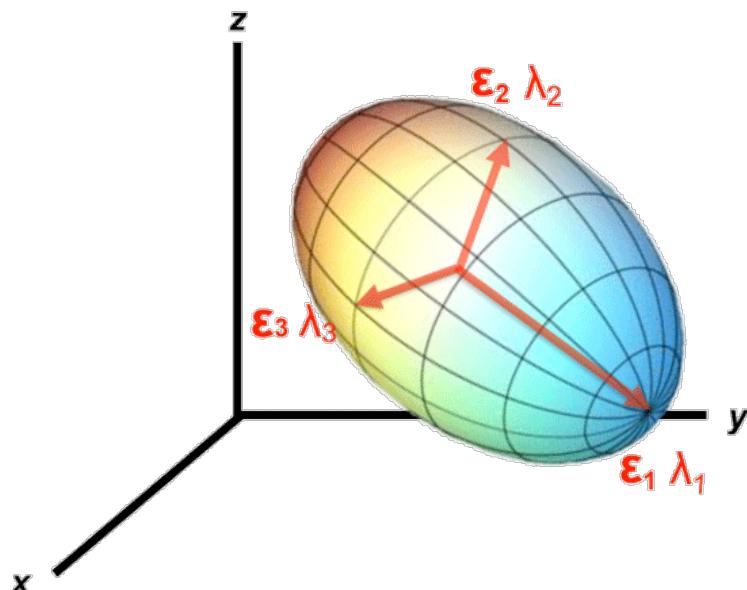
Diffusion tensor

Fortunately an ideal frame of reference for viewing the diffusion tensor exists and can be determined using measurements obtained from any frame of reference. This optimal coordinate system is based upon the **diffusion ellipsoid**, whose main axis is parallel to the principal diffusion direction within a voxel. This principal axis often corresponds to anatomic features such as white matter tracts or fascial planes.

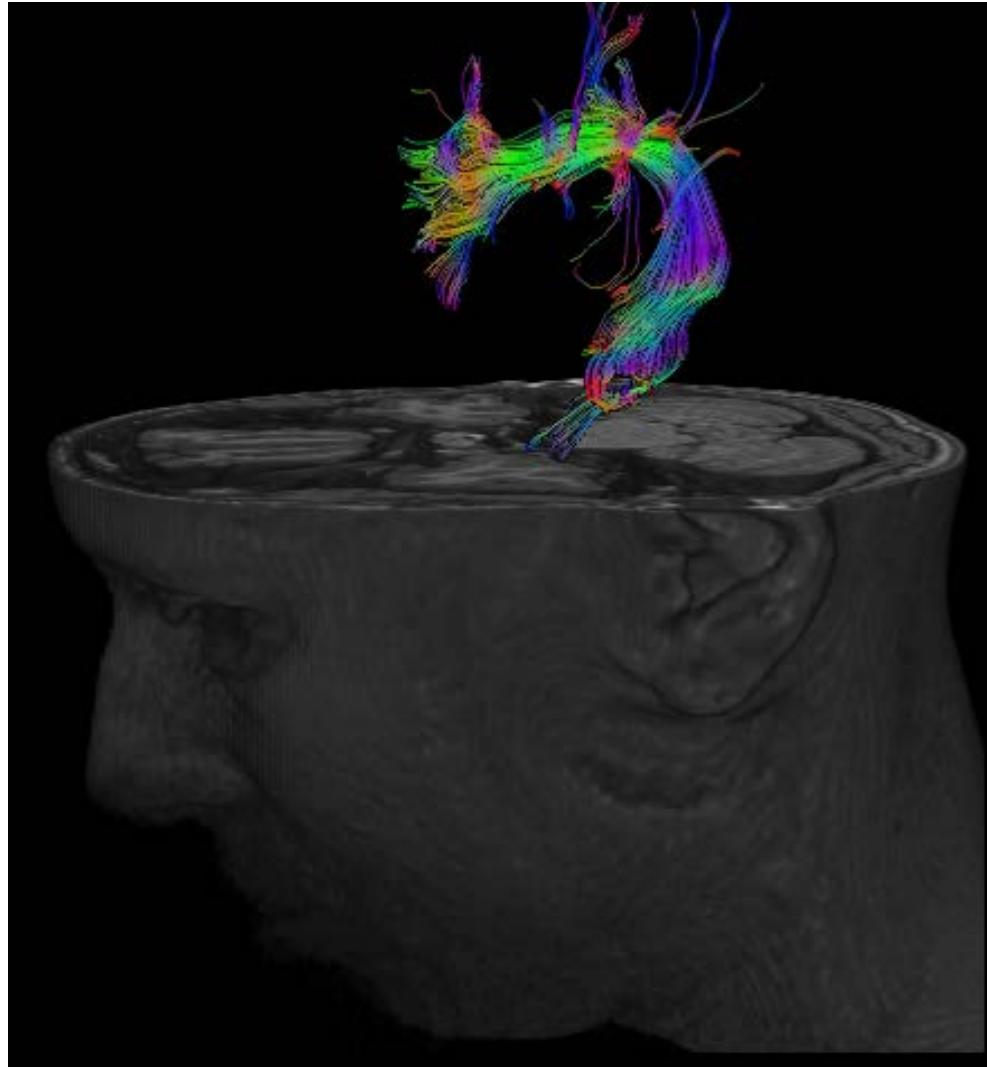


Diffusion tensor

The major and minor axes of the diffusion ellipsoid are defined by three orthogonal unit vectors (ε_1 , ε_2 , and ε_3) known as **eigenvectors**. The length of each eigenvector (ε_i) is multiplied by a factor λ_i , called the **eigenvalue**. The eigenvalues of the ellipsoid are proportional to Einstein's root mean squared diffusion displacement in each direction. By convention, eigenvalues are labeled in descending order of magnitude ($\lambda_1 \geq \lambda_2 \geq \lambda_3$).



Fiber Tracking (tractography)



Novell trends in MRI

- Canon
- GE
- Philips
- Siemens

Helium free

The infographic highlights the following features of the MAGNETOM Free.Max 1.5T X:

- New clinical fields (lungs icon)
- Minimal distortions with implants (implant icon)
- Widest bore improves patient experience (80 cm bore width icon)
- 0.7 l liquid Helium (He symbol)
- myExam companion assists user with AI (brain icon)
- MAGNETOM Free.Max¹** (central title)
- No quench pipe necessary (X icon)
- Image quality comparable to higher field strengths (camera icon)
- Lightest MR < 3.2 tons (scale icon)
- Smallest MR < 2 m height (upward arrow icon)
- Unique combination of digital technologies and new field strength of 0.55 Tesla (coil icon)

MAGNETOM Free.Max is still under development and not commercially available yet. Its future availability cannot be ensured.



PRESS RELEASE

Setting Helium Free: Revolutionary MRI Tech from GE Healthcare

Freelium, a magnet technology, designed to use 20 liters of liquid helium instead of 2,000 liters

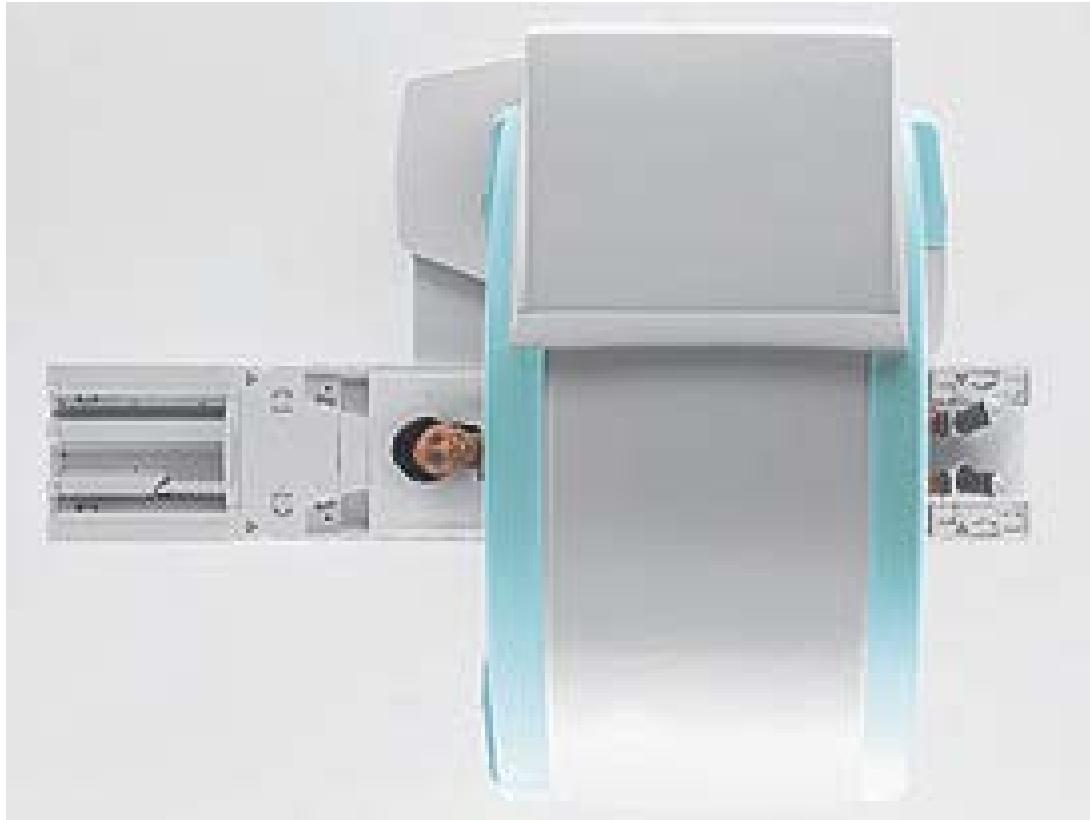
CHICAGO - November 29, 2016 - Helium, a critical component in magnetic resonance imaging (MRI) systems, has gone through two potential shortage crises, impacting hospitals and patients around the globe. But the helium supply is finite and demand has been rising over the past decades. At #RSNA16, GE Healthcare (NYSE: GE) proudly unveils Freelium*, a magnet technology designed to use one percent of liquid helium compared to conventional MRI magnets. Instead of the average 2,000 liters of precious liquid helium, Freelium is designed to use only about 20 liters.

Ingenia Ambition 1.5T X

Excel in your daily MR services, helium-free
[Najít podobné výrobky ›](#)

Based on its new, revolutionary fully sealed BlueSeal magnet, Ingenia Ambition X lets you experience more productive¹ helium-free MR operations. The Ingenia Ambition X delivers superb image quality even for challenging patients, and performs MRI exams up to 50% faster² with Compressed SENSE accelerations for all anatomies, in both 2D- and 3D scanning. Fast overall exam-time is achieved by simplifying patient handling at the bore with the touchless guided patient setup. Furthermore, the Ingenia Ambition offers an immersive audio-visual experience to help calm patients and guide them through MR exams.

Patient's comfort



unique **over-sized bore opening** and **short magnet design** delivers the most comfortable patient experience available along with exceptional imaging results – ***Claustrophobia v. magnetic field homogeneity.***

Strong magnetic field – $B_0 + \text{grad.}$



System weight (in operation)

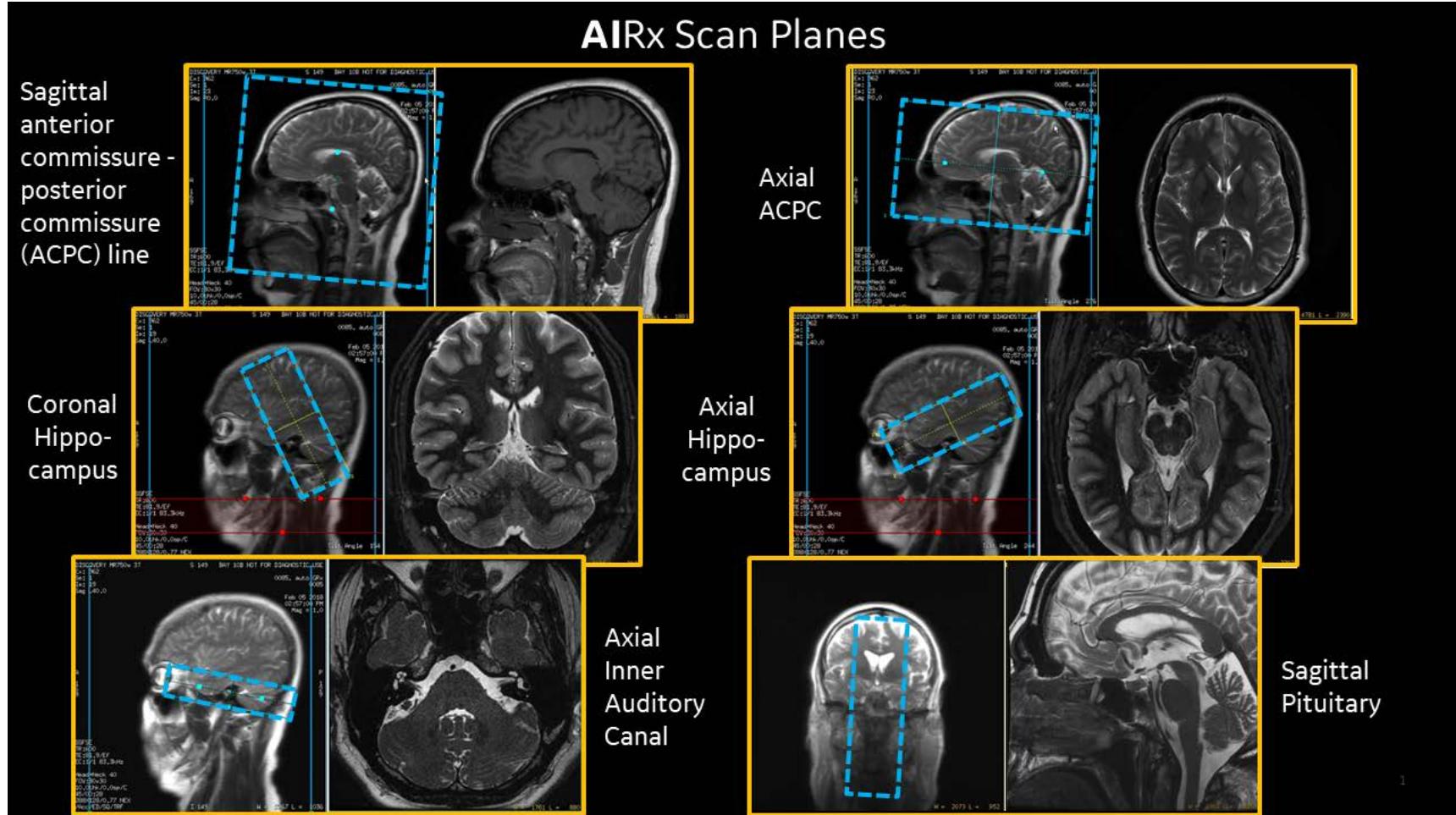
<25 tons

Flexible coils



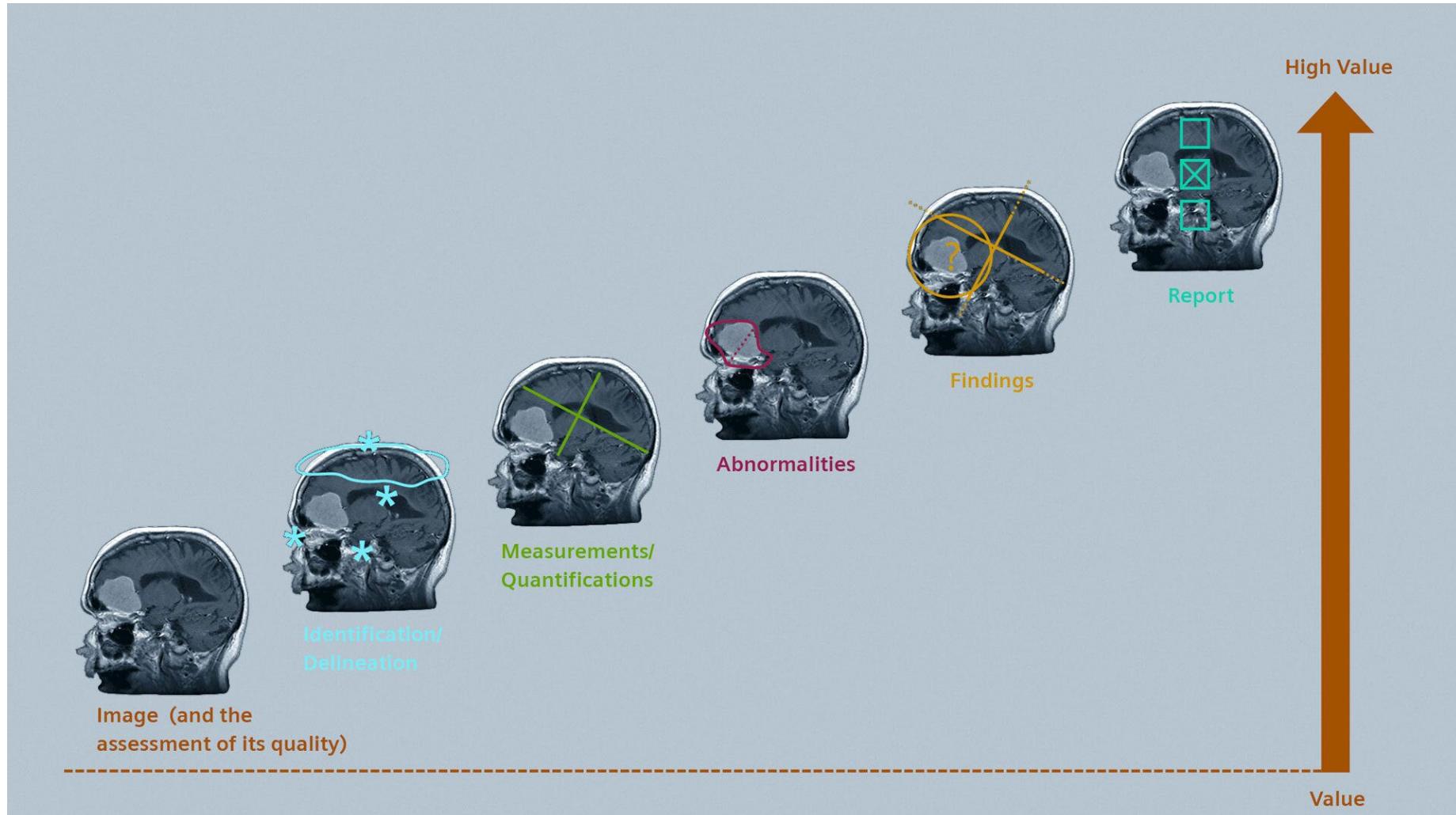
<https://magnetismag.com/ges-flexible-coils-receiving-favorable-user-reviews-in-mri-procedures/>

Artificial intelligence in MRI



[1](http://newsroom.gehealthcare.com>this-ai-tech-is-changing-mr-neuro-imaging/</p></div><div data-bbox=)

Artificial intelligence in MRI



Použité zdroje

- Magnetic Resonance Imaging - Siemens Healthineers, 2023 [online]. [cit. 29. 9. 2019]. Dostupné z: <https://www.siemens-healthineers.com/magnetic-resonance-imaging/>
- MRI Questions, 2023 [online]. [cit. 29. 9. 2019]. Dostupné z: <https://www.mriquestions.com/index.html>
- The Basics of MRI, 2023 [online]. [cit. 29. 9. 2019]. Dostupné z: <https://www.cis.rit.edu/htbooks/mri/>
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- BME 595 – Medical Imaging Applications Part 2: Introduction to MRI. 2023 [online]. [cit. 29. 9. 2019]. Dostupné z: <https://www.slideshare.net/SanjeebSinha3/mri1ppt>
- BUSHBERG, Jerrold T. The essential physics of medical imaging [online]. Third edition. Philadelphia: Wolters Kluwer Health/Lippincott Williams & Wilkins, [2012], ©2012 [cit. 2019-09-29]. Dostupné z: <<https://ebookcentral.proquest.com/lib/cvut/detail.action?docID=2031899>>.